

# Modeling variability in cardiac electrophysiology

GDR Mamovi, Lyon  
September 28, 2017

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## Joint work with:



Damiano Lombardi  
(Inria)



Elliott Tixier  
(Inria)

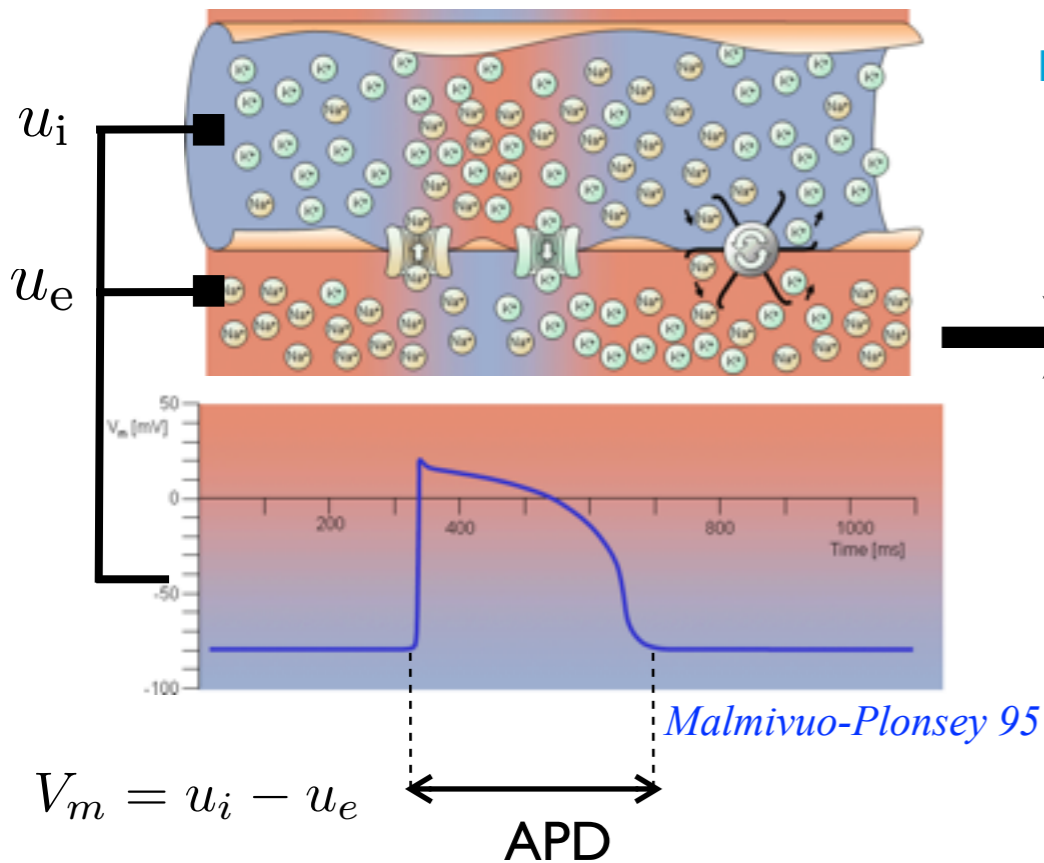


Blanca Rodriguez  
(Oxford Univ.)

# Electrocardiograms

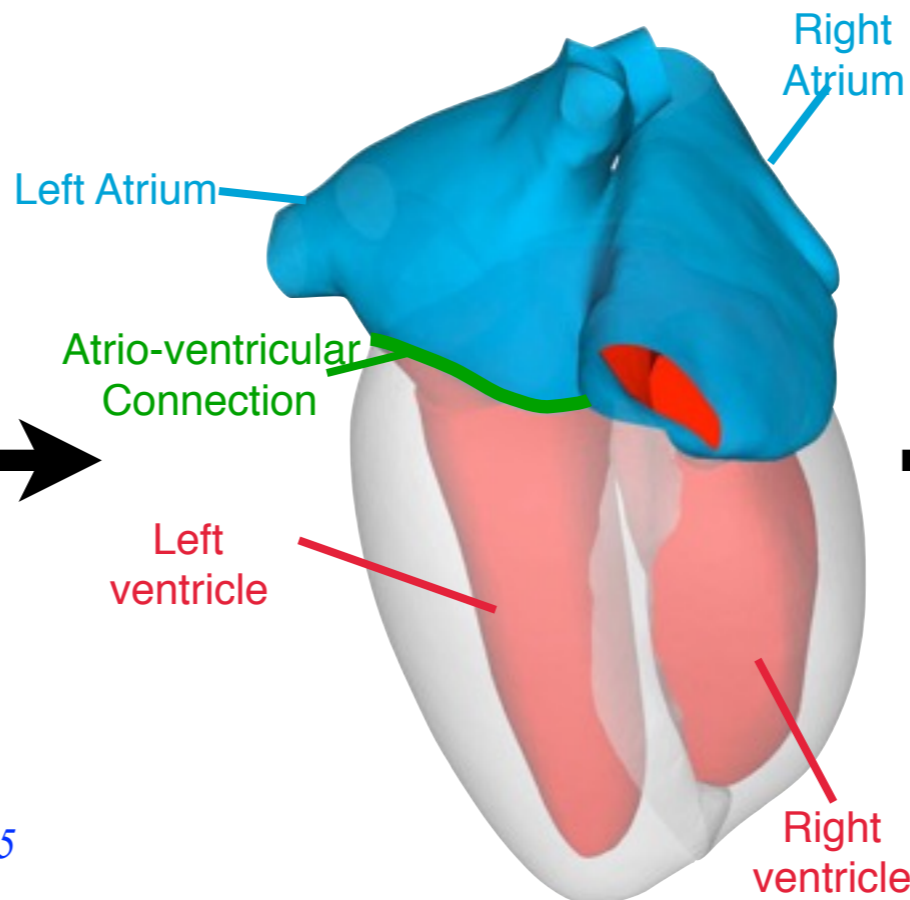
## Cell scale:

Hodgkin-Huxley-like models



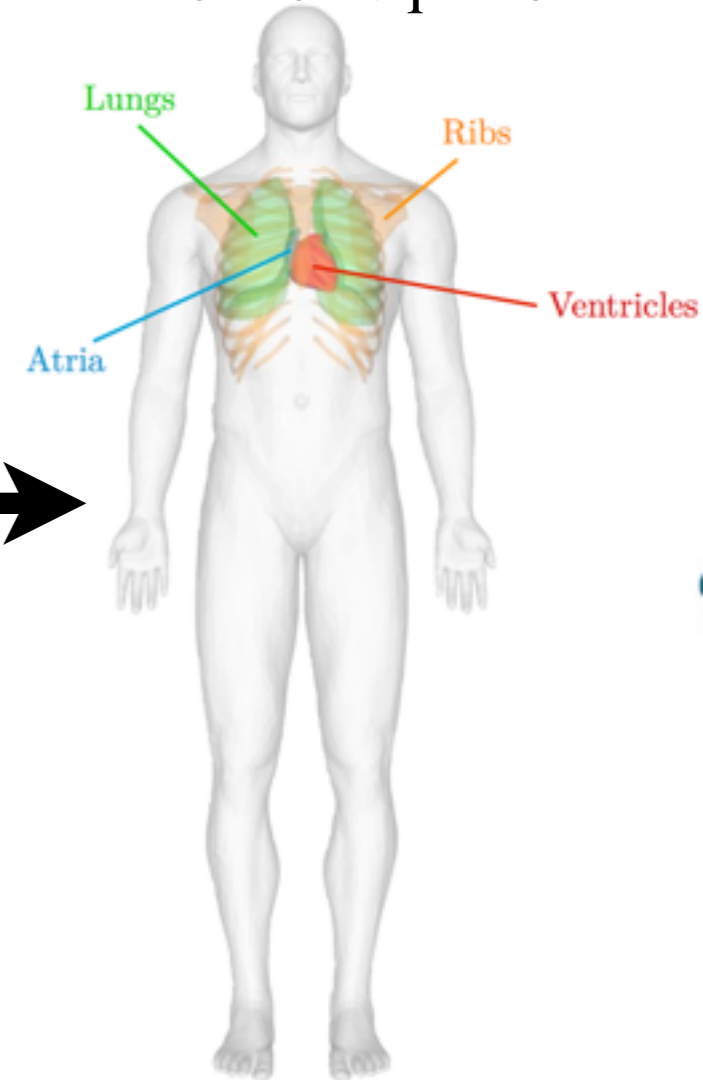
## Myocardium:

bidomain models



## Torso:

Poisson equation



$$\begin{cases} C_m \frac{dV_m}{dt} + I_{\text{ion}}(V_m, \mathbf{g}) = 0 \\ \frac{d\mathbf{g}}{dt} + G(V_m, \mathbf{g}) = 0 \end{cases}$$

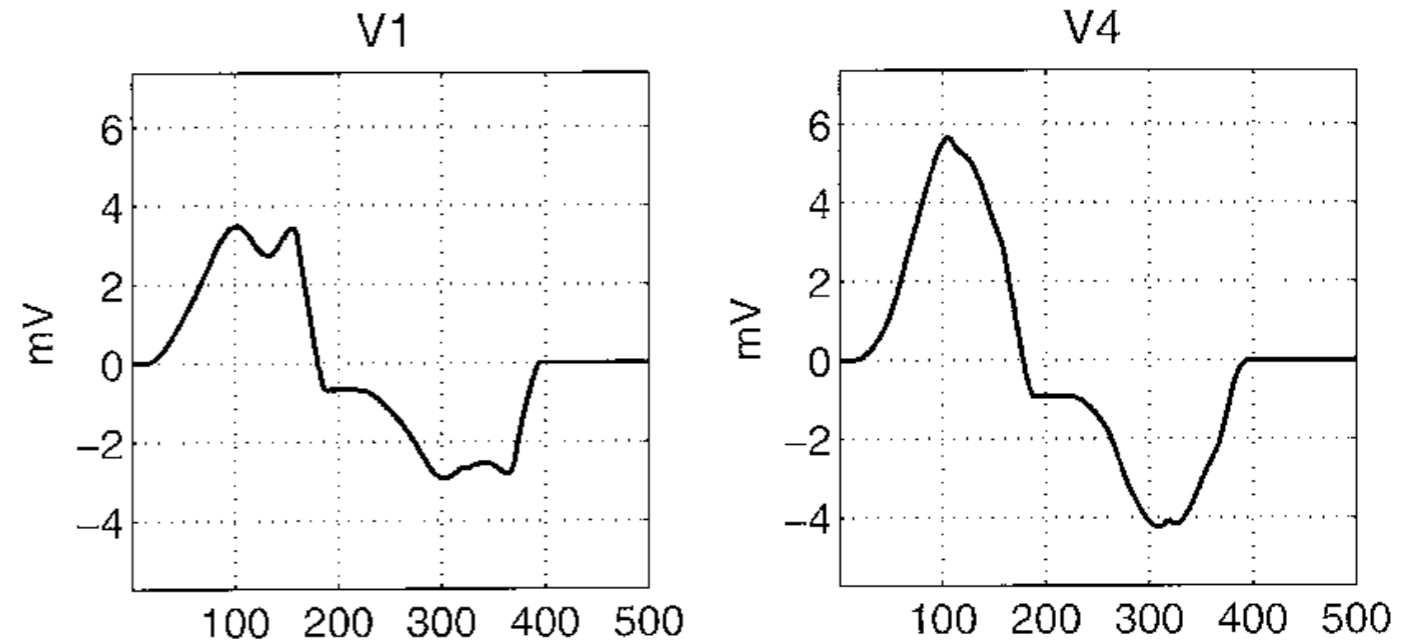
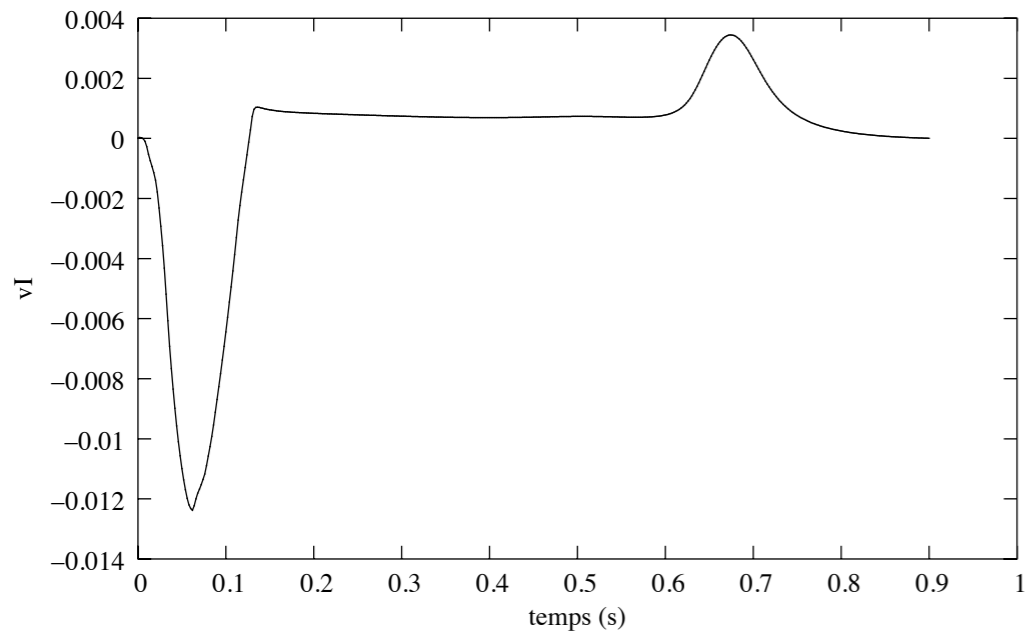
$$\begin{cases} A_m \left( C_m \frac{\partial V_m}{\partial t} + I_{\text{ion}}(V_m, \mathbf{g}) \right) - \text{div}(\boldsymbol{\sigma}_i \nabla u_i) = A_m I_{\text{app}}, \\ \text{div}(\boldsymbol{\sigma}_e \nabla u_e) + \text{div}(\boldsymbol{\sigma}_i \nabla u_i) = 0 \\ \frac{\partial \mathbf{g}}{\partial t} + G(V_m, \mathbf{g}) = 0, \end{cases}$$

$$\begin{cases} \text{div}(\boldsymbol{\sigma}_T \nabla u_T) = 0 \\ + \text{transmission condition} \\ \text{on the epicardium} \end{cases}$$



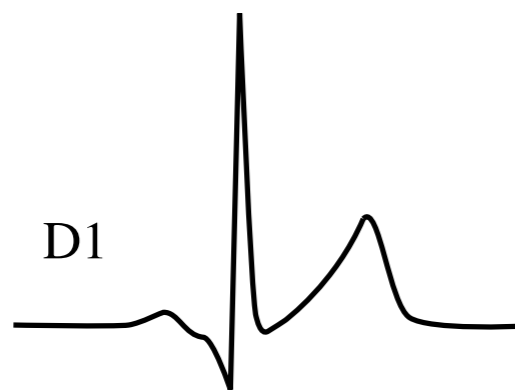
e.g.: Pullan et al. 05, Sundes et al. 06, ...  
Boulakia, Cazeau, Fernández, JFG, Zemzemi, *Annals Biomed Engng* 2010

# First results...



*(Sundnes et al., Springer 2006)*

In 2007...



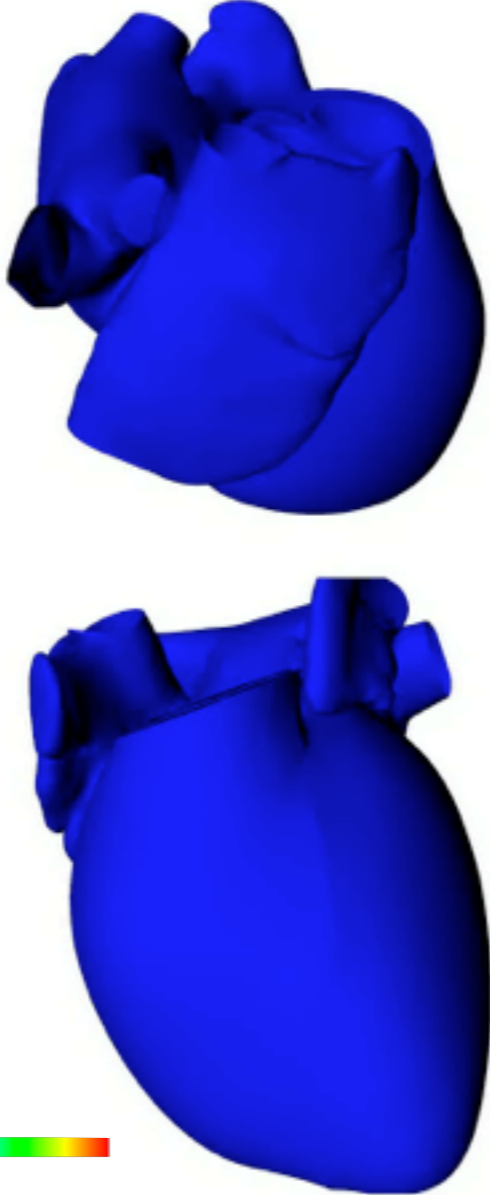
V1

V4

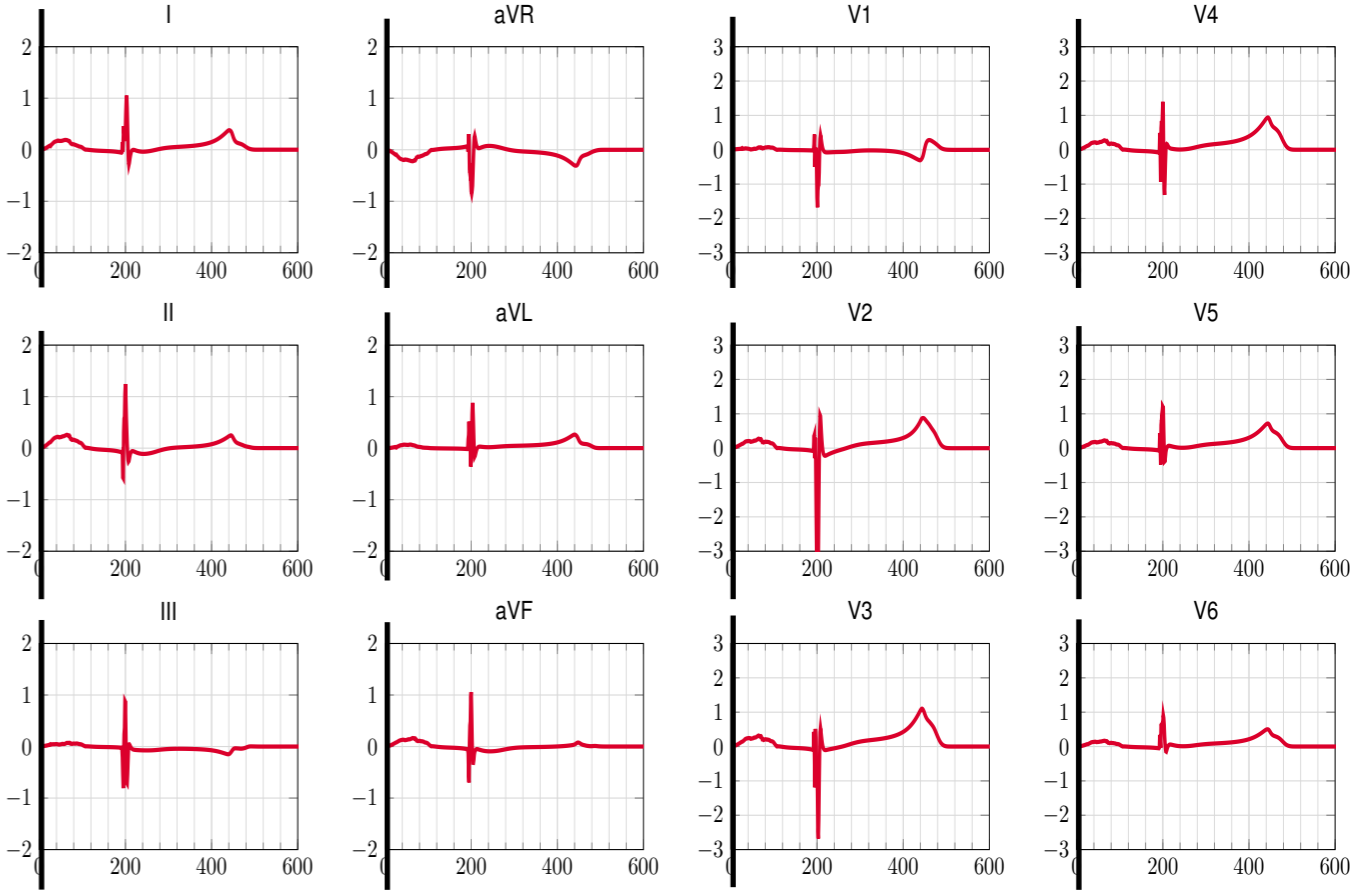
# Standard 12-lead ECG



Body Potential  $u_T$  (mV)  
-1.0    0.0



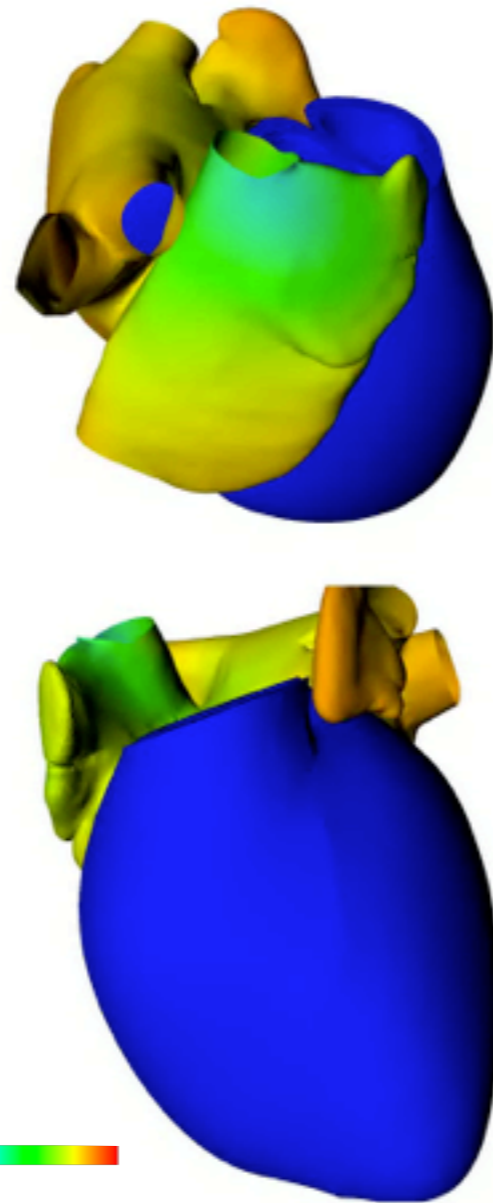
Transmembrane Potential  $V_m$  (mV)  
-80.0    20.0



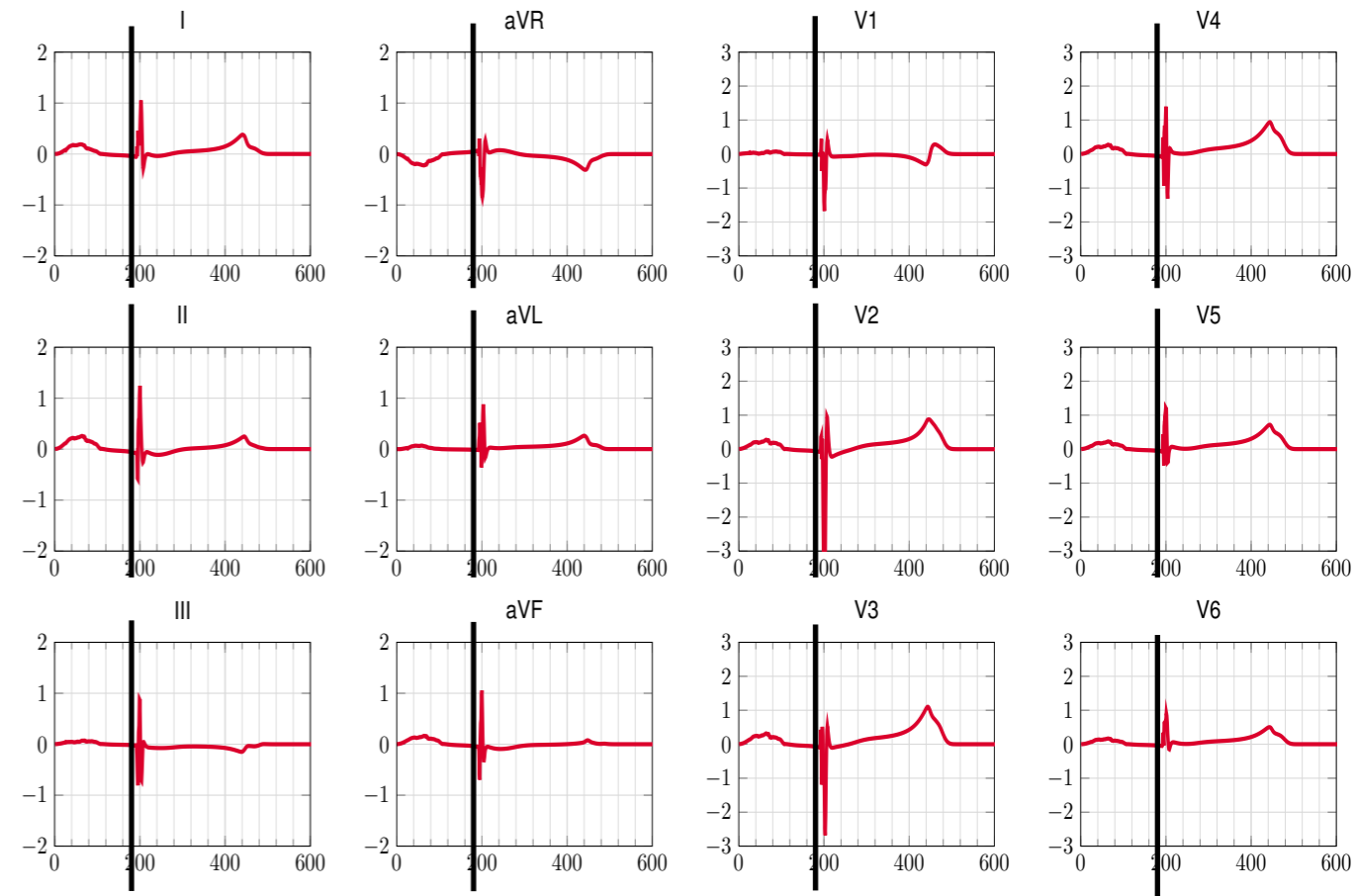
# Standard 12-lead ECG

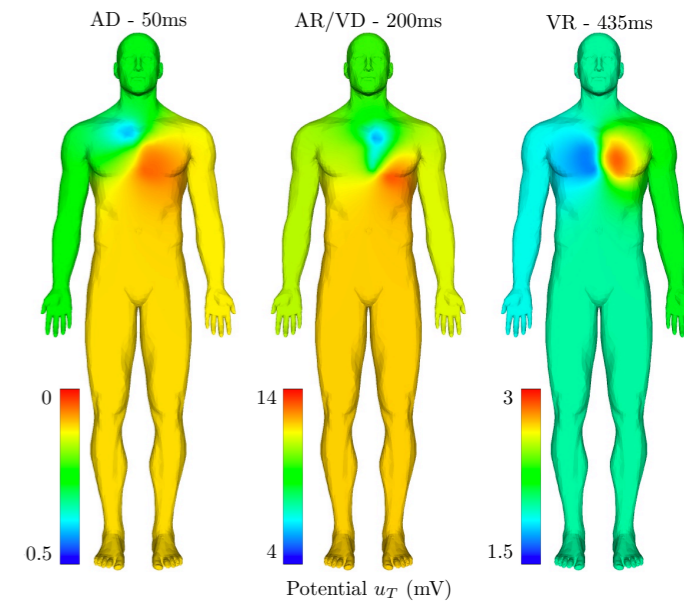
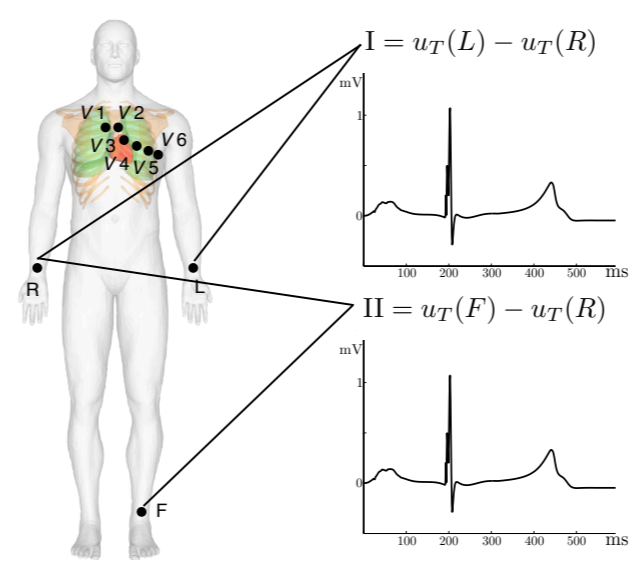
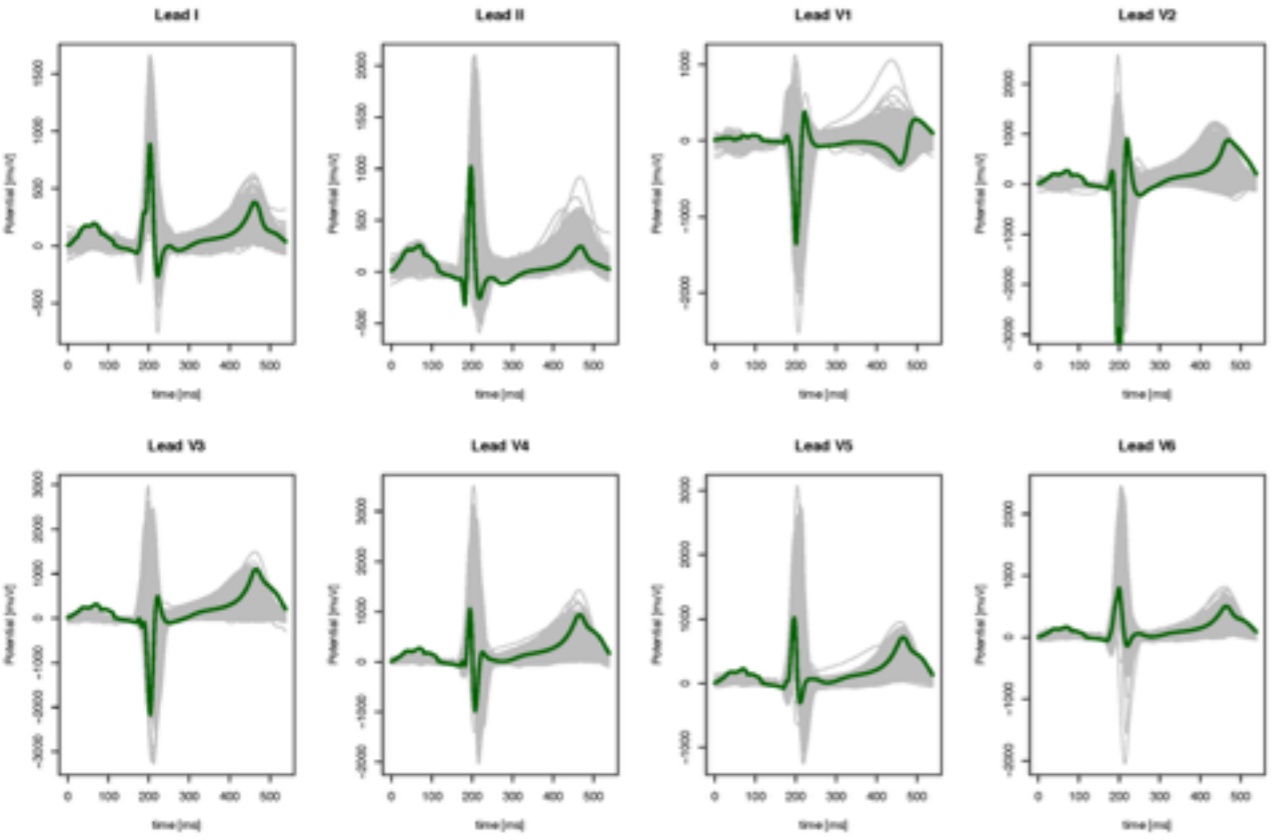


Body  
Potential  $u_T$  (mV)  
0.0 10.0



Transmembrane  
Potential  $V_m$  (mV)  
-80.0 20.0

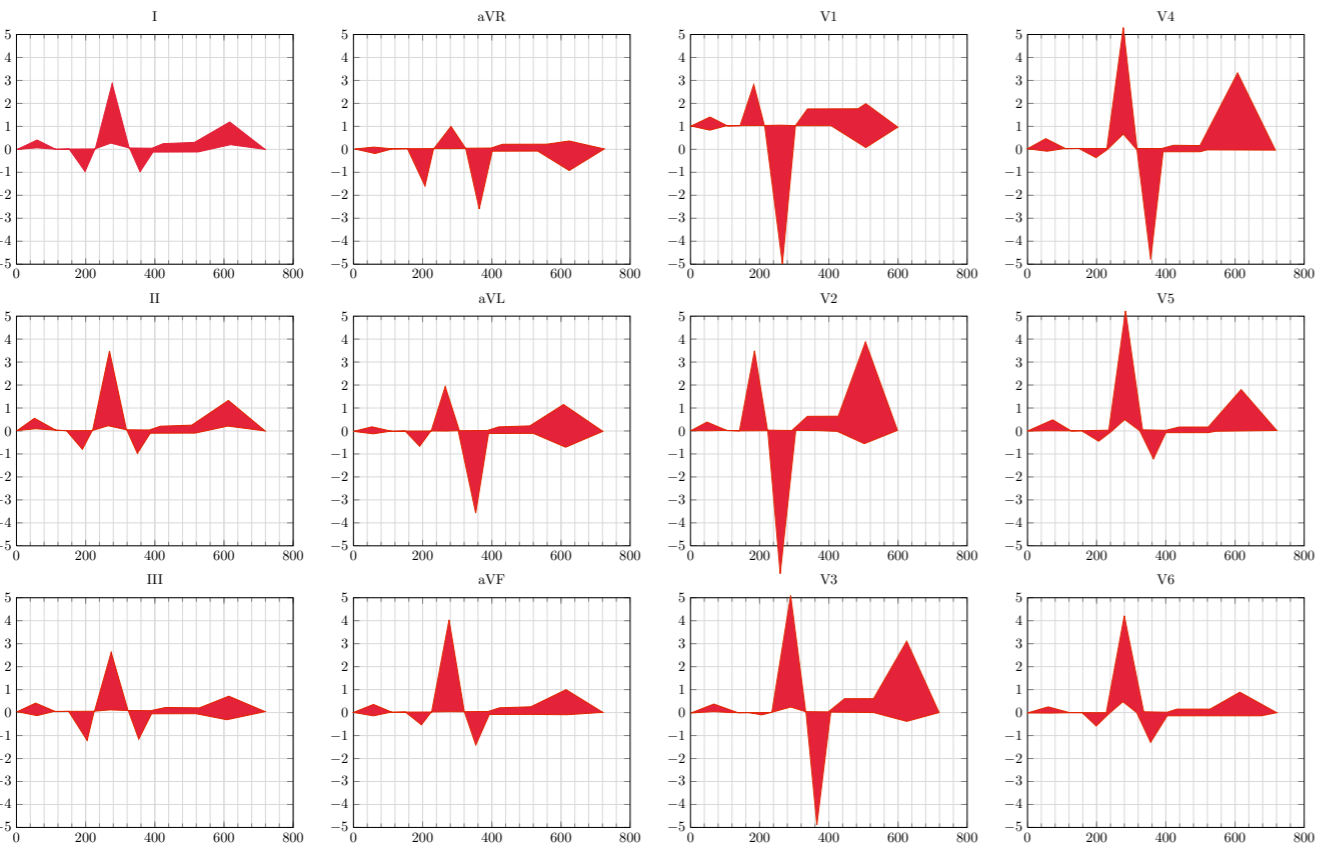




*ECG Simulation*

	P wave	PR interval	Q wave	QR interval	S wave	QRS interval	QT interval
Typical ECG	< 0.12	0.12 to 0.21	< 0.04	< 0.03 V1-V2 < 0.05 V5-V6	< 0.04	< 0.10	0.35 to 0.45
Healthy Simul.	0.08	0.19	0.015	0.015 V1-V2 0.02 V5-V6	0.01	0.04	0.29

*N.Tarabelloni, A.M.Paganoni & F.Ieva (Politecnico di Milano)*



*“normal ECGs” (from Joseph Wartak)*

Wave/Interval	Description	Simulated ECG
P wave	$\leq 0.25\text{mV}$ positive I, II, V3 to V6 negative aVR	✓ 0.2mV ✓
Q wave	limb leads $\leq 25\%$ of R precordial leads $\leq 15\%$ of R always negative	✓ ✓ ✓ except for aVL
R wave	limb leads $\leq 2\text{mV}$ precordial leads $\leq 3\text{mV}$ always positive, negative in aVR R wave progression, see Figure 12	✓ ✓ ✓ ✓
S wave	always negative small I, II, V5, V6 important V1 to V3	✓ ✓ ✓
ST interval	$-0.05\text{mV}$ to $0.1\text{mV}$ isoelectric displacement of $0.02\text{mV}$ in V1, V3	✓ ✓ ✓
T wave	positive I, II, V3 to V6 negative aVR (follow the QRS)	✓ ✓

# Variability modeling

## Our goal:

- Given measurements in a population of individuals
- Infer a probability density function (pdf) for some parameters

## Standard approaches:

- Solve an inverse problem for each individual separately
- Population approach:
  - consider all the individuals together
  - look for average population parameters, standard deviation, ...



E Kuhn, M Lavielle, “Maximum likelihood estimation in nonlinear mixed effects models”, [Comp Stat Data Analysis, 2005](#).



E Grenier, V Louvet, P Vigneaux, “Parameter estimation in non-linear mixed effects models with SAEM algorithm: extension from ODE to PDE”, [M2AN, 2013](#).



# Variability modeling

## Our wishes:

- Non-intrusive: black box algorithm
- Non-parametric: no assumption on the distribution
- Moderate number of model evaluations

## Our approach:

- Match the *moments* of the “*observables*” and of the measurements

# Variability modeling: moments matching

- Hausdorff moment problem:
  - find a distribution given its moments

$$m_j = \int_{\Theta} \theta^j \rho(\theta) d\theta$$

- in general, an ill-posed problem
- Regularization: **Maximum Entropy Principle** (Jaynes, 1957)
  - Maximises the Shannon entropy:

$$S(\rho) = - \int_{\Theta} \rho(\theta) \log(\rho(\theta)) d\theta$$

Under the constraints defined by the available information

# Examples

- Information:

- $X$  a random variable with values in  $[a, b]$

Maximum Entropy Principle  $\implies \rho$  is a uniform pdf on  $[a, b]$

- Information:

- $X$  a random variable with values in  $\mathbb{R}_+^*$
- $\mathbb{E}(X) < +\infty$  given
- $\mathbb{E}(\log(X)) < +\infty$  given.

Maximum Entropy Principle  $\implies \rho$  is a Gamma pdf

- Information:

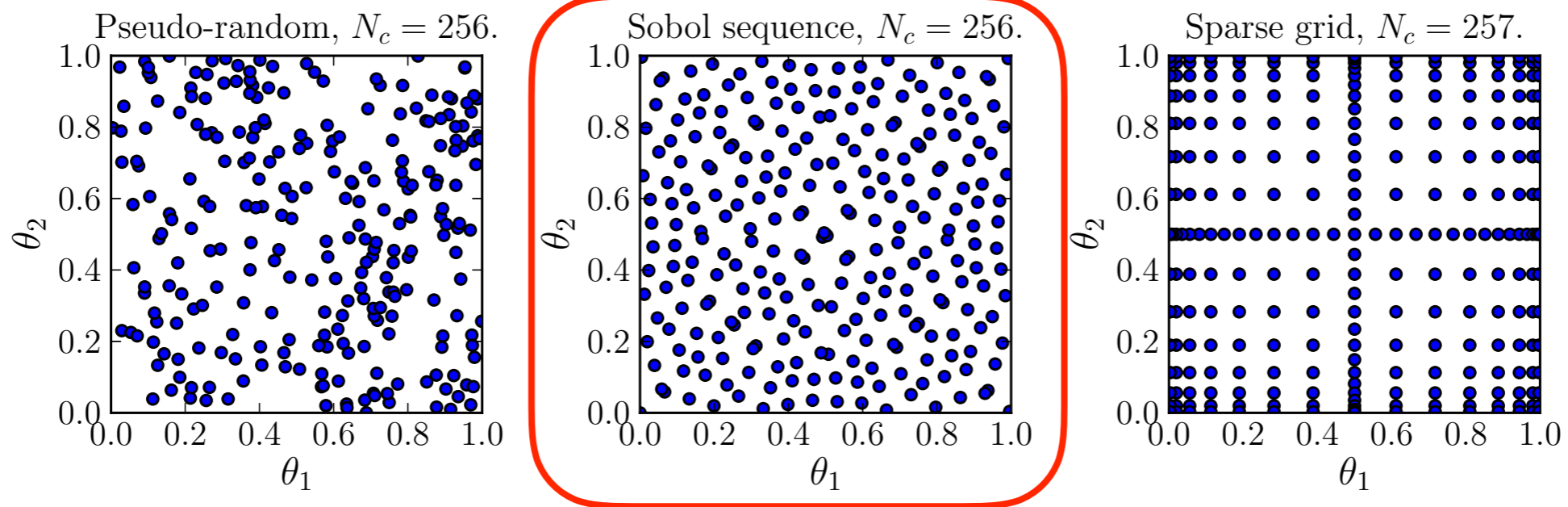
- $X$  a random variable with values in  $\mathbb{R}$
- $\mathbb{E}(X) < +\infty$  given
- $\mathbb{E}(X^2) < +\infty$  given

Maximum Entropy Principle  $\implies \rho$  is a Gaussian pdf



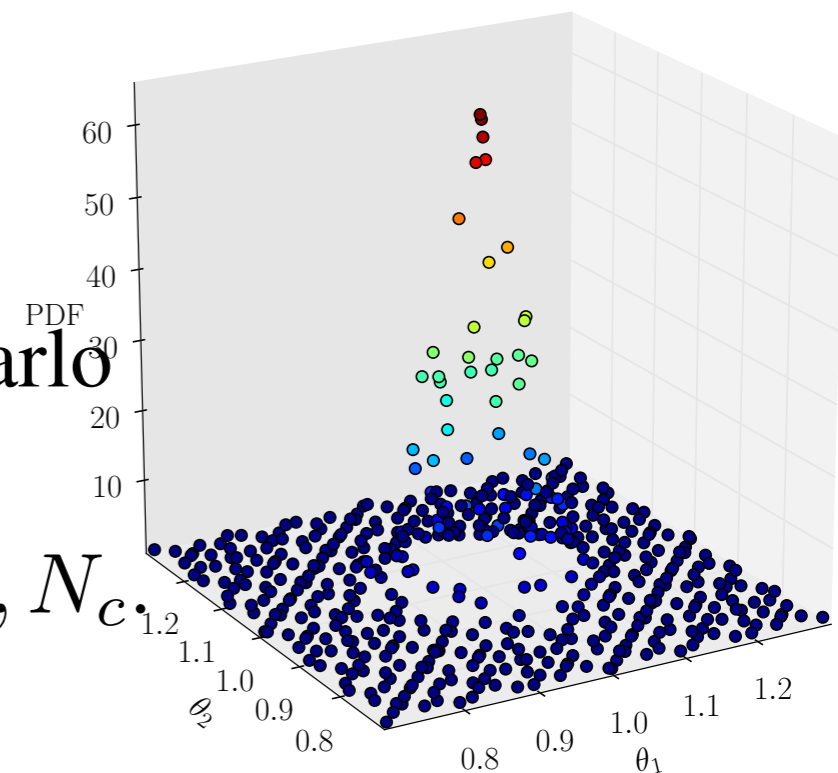
# Observable Moments Matching

- Sampling:  $\theta_i \in \Theta, i = 1, \dots, N_c$



→ Sobol sequence in the parameter space.

- The model is evaluated on each  $\theta_i$  (*off-line*)
- Integrals over  $\Theta$  approximated by quasi-Monte-Carlo
- We look for an approximation of  $\rho(\theta_i), i = 1, \dots, N_c$ .



# Observable Moments Matching

- Maximize the **entropy**  $S(\rho) = -\int_{\Theta} \rho \log(\rho)$  under the constraints

$$c_{\rho}(\mathbf{x}_j, m) = \mu_m^{\rho}(\mathbf{x}_j, m) - \hat{\mu}_m(\mathbf{x}_j, m) = 0, \text{ for } N_k \text{ points } \mathbf{x}_j \in \mathcal{D}$$

- Saddle-point problem:  $\inf_{\rho} \sup_{\lambda, \lambda_0, \nu \geq 0} \mathcal{L}(\rho, \lambda, \lambda_0, \nu)$

$$\mathcal{L}(\rho, \lambda, \nu) = \underbrace{\int_{\Theta} \rho \log(\rho)}_{-S(\rho)} - \sum_{j=1}^{N_k} \sum_{m=1}^{n_{mom}} \lambda(\mathbf{x}_j, m) \underbrace{c_{\rho}(\mathbf{x}_j, m)}_{\text{mom. cons.}} - \lambda_0 \underbrace{\left( \int_{\Theta} \rho - 1 \right)}_{\text{normalization}} - \underbrace{\int_{\Theta} \rho \nu}_{\text{positivity}}.$$

- “Inf” step done analytically. Positivity constraint automatically verified
- “Sup” step done numerically using quasi-Newton method
- Dense linear system of size  $(N_k n_{mom}) \times (N_k n_{mom})$

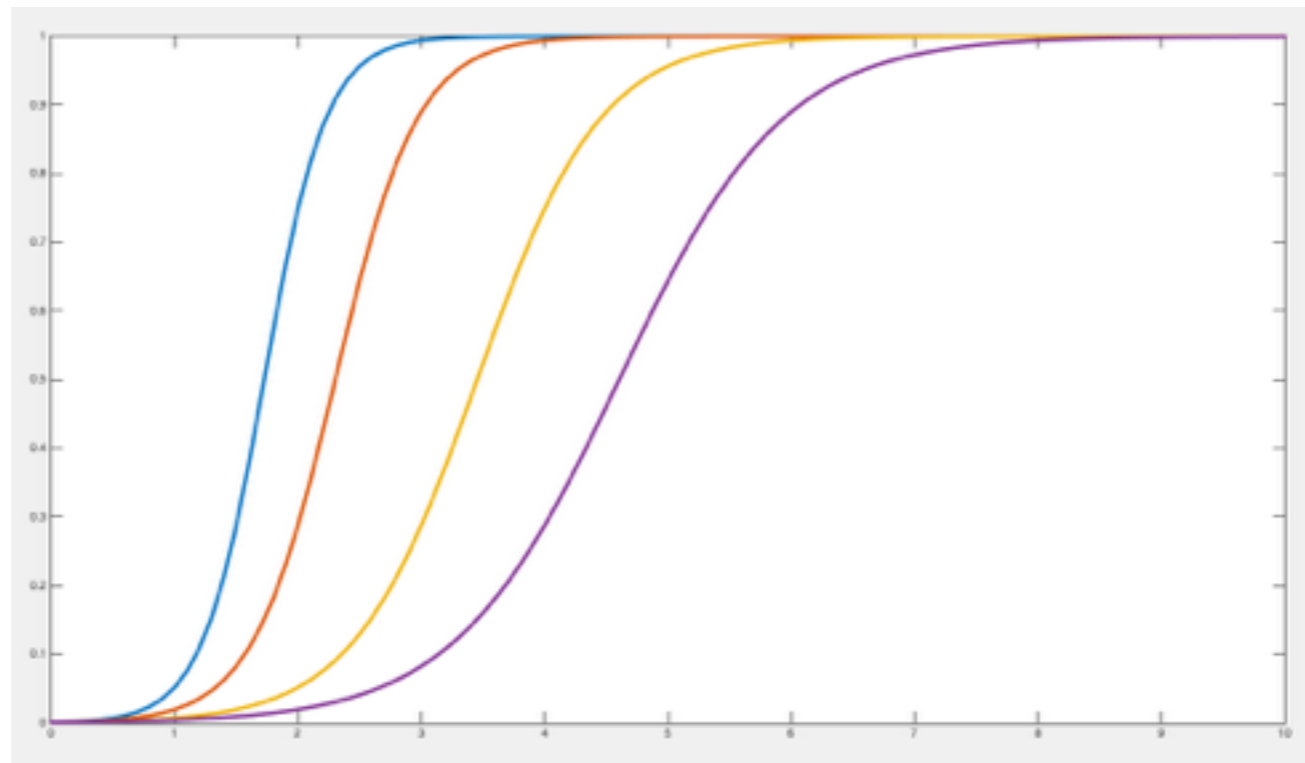
# Selection of physical points: sensitivity

## Issue

- Too many points in the physical space
- Many points are redundant: **big and ill-conditioned problem**

## Illustrative example

- Logistic equation  $\frac{du}{dt} = k u(1 - u)$  for different values of  $k$



# Selection of physical points: sensitivity

## Strategy

- Quantify how the parameters affect the variability at a given  $\mathbf{x}_j$ .
- Sensitivity Gramm matrix, using the model outputs:

$$\mathbf{C}(\mathbf{x}_j) = \int_{\Theta} [\nabla_{\theta} g(\mathbf{x}_j, \theta)] [\nabla_{\theta} g(\mathbf{x}_j, \theta)]^T \rho(\theta) d\theta$$

estimated *off-line*

start with a guess  
then iterate

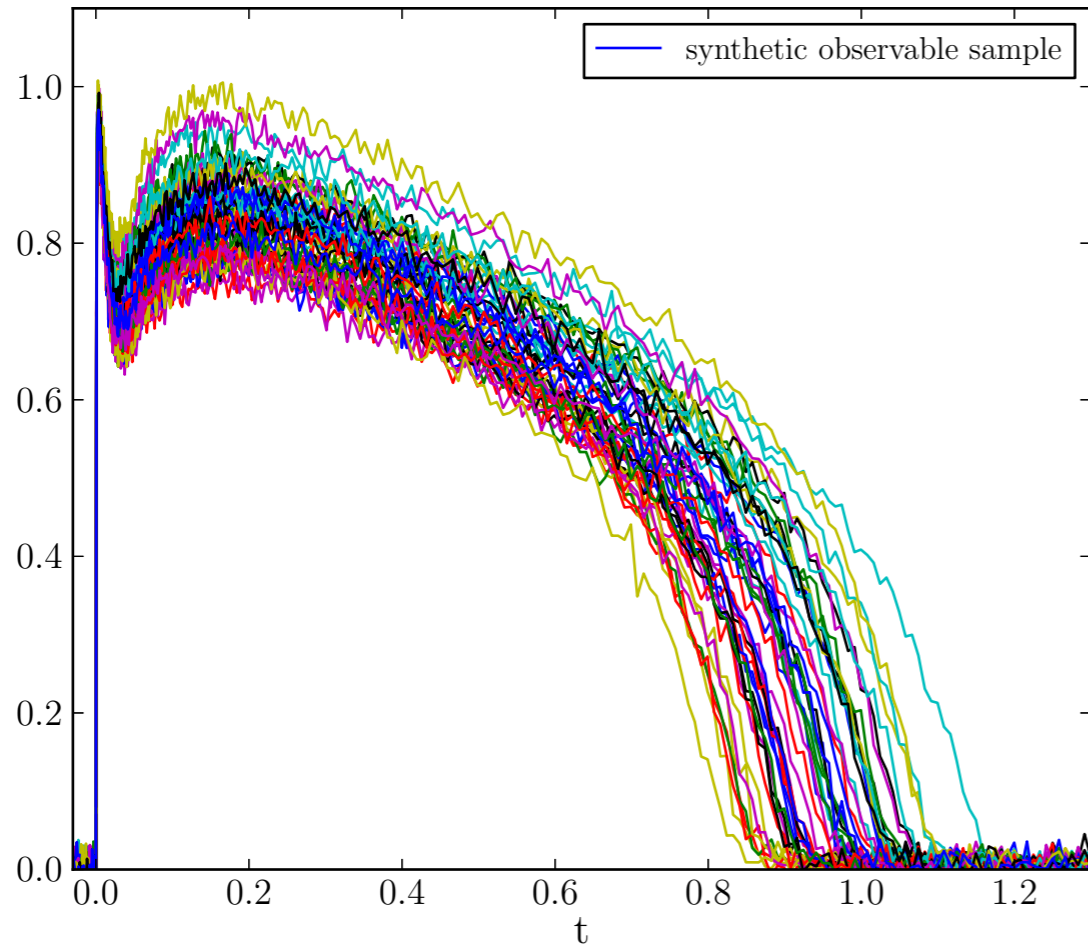
- Eigenvalue decomposition of  $\mathbf{C}(\mathbf{x}_j)$ :  $\lambda_{j,k}, \mathbf{e}_{j,k}$
- $\mathbf{e}_{j,1}$  = direction in  $\Theta$  of maximum variation on average
- $\lambda_{j,1}$ : mean-squared derivative of the observable along the direction  $\mathbf{e}_{j,1}$



# Selection of physical points: clustering

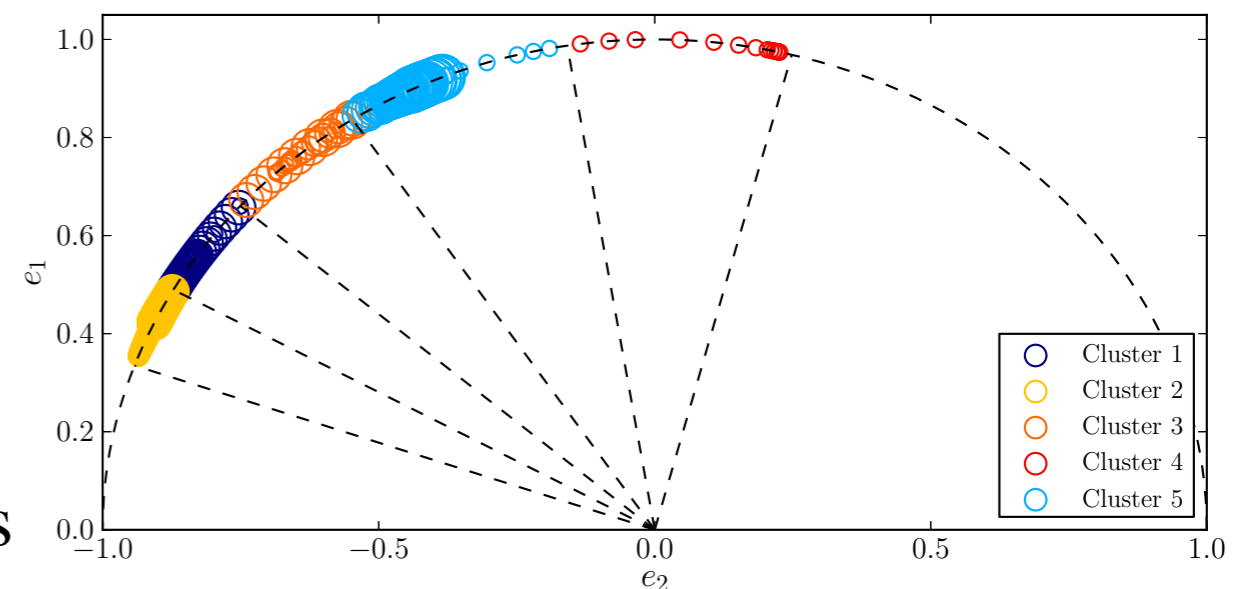
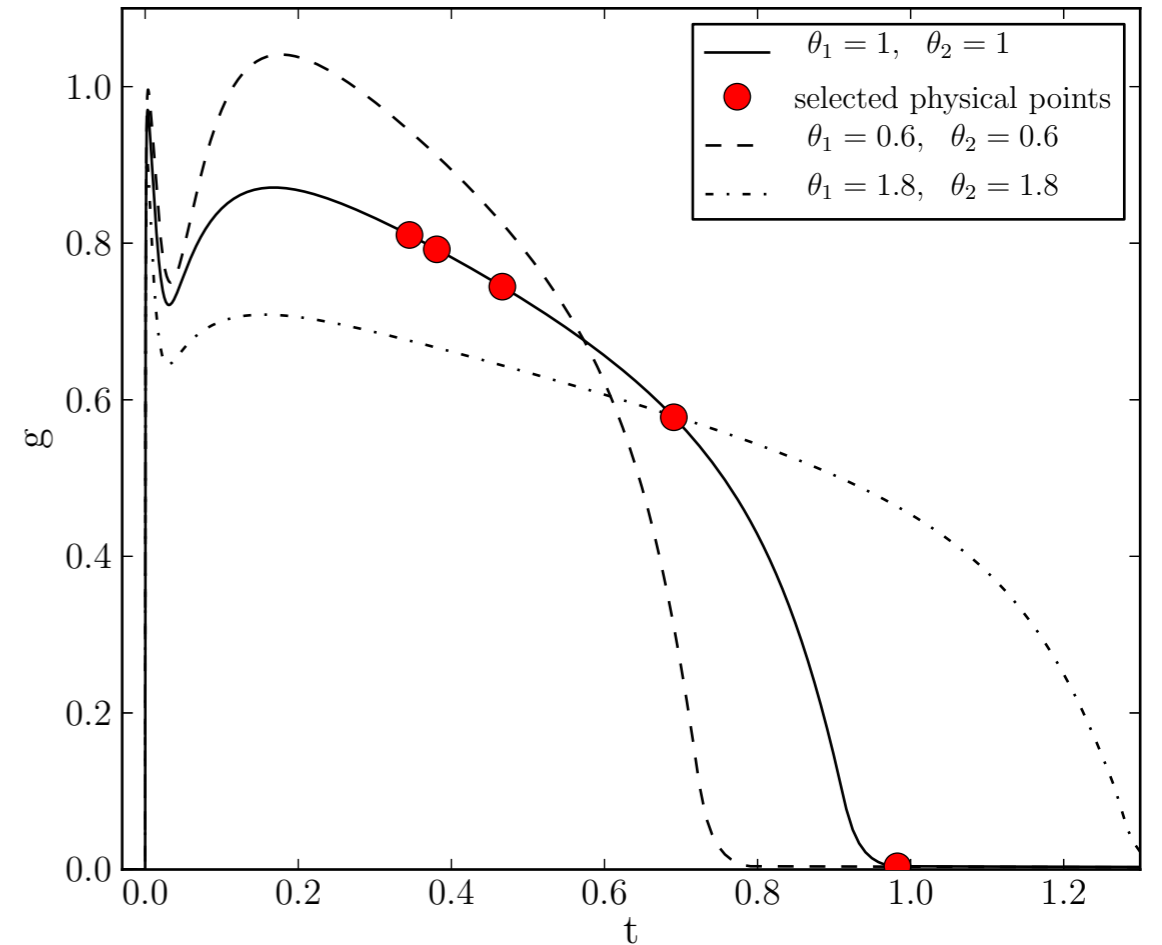
- Points with similar dominant directions are considered as redundant
- Agglomerative hierarchical **clustering algorithm**
- The  $N_{\mathbf{x}}$  points of the full physical set are divided into  $N_k$  clusters
- Points with maximum trace of  $\mathbf{C}(\mathbf{x}_j)$  are chosen as cluster representative
- Subset  $\mathcal{S}$  where the moments are matched: the  $N_k$  representatives

# Example with an ODE



Cardiac cell Action Potential

- Two parameters  $\theta_1, \theta_2$
- $N_c = 1024$  Sobol points in  $[0.6, 1.8]^2$
- $N_x = 334$  time instants,  $N_k = 5$  clusters



First eigenvectors of the Sensitivity Gram Matrices at each time instants

# Algorithm

- Initial guess:  $\rho^{(0,0)}$  uniform density over  $\Theta$
- $j = 1$
- While  $\|R(\rho^{(j-1,0)})\| \geq \text{tol}$ 
  - **Clustered Sensitivities** with  $\rho^{(j-1,0)}$   
 $\implies$  nested subsets  $\mathcal{S}^k$  of  $k$  physical points
  - $n = 1$
  - While  $\|R(\rho^{(j-1,n-1)})\| \geq \text{tol}$ 
    - **Observable Moments Matching** on  $\mathcal{S}^n$   
 $\implies \rho^{(j-1,n)}$
    - $n \leftarrow n + 1$
  - $\rho^{(j,0)} \leftarrow \rho^{(j-1,n)}$
  - $j \leftarrow j + 1$
- $n_{iter} = j$

## Remarks:

- Residual on **all the**  $N_x$  physical points:

$$R(\rho) = \sum_{j=1}^{N_x} \sum_{m=1}^{n_{mom}} c_\rho(\mathbf{x}_j, m)^2$$

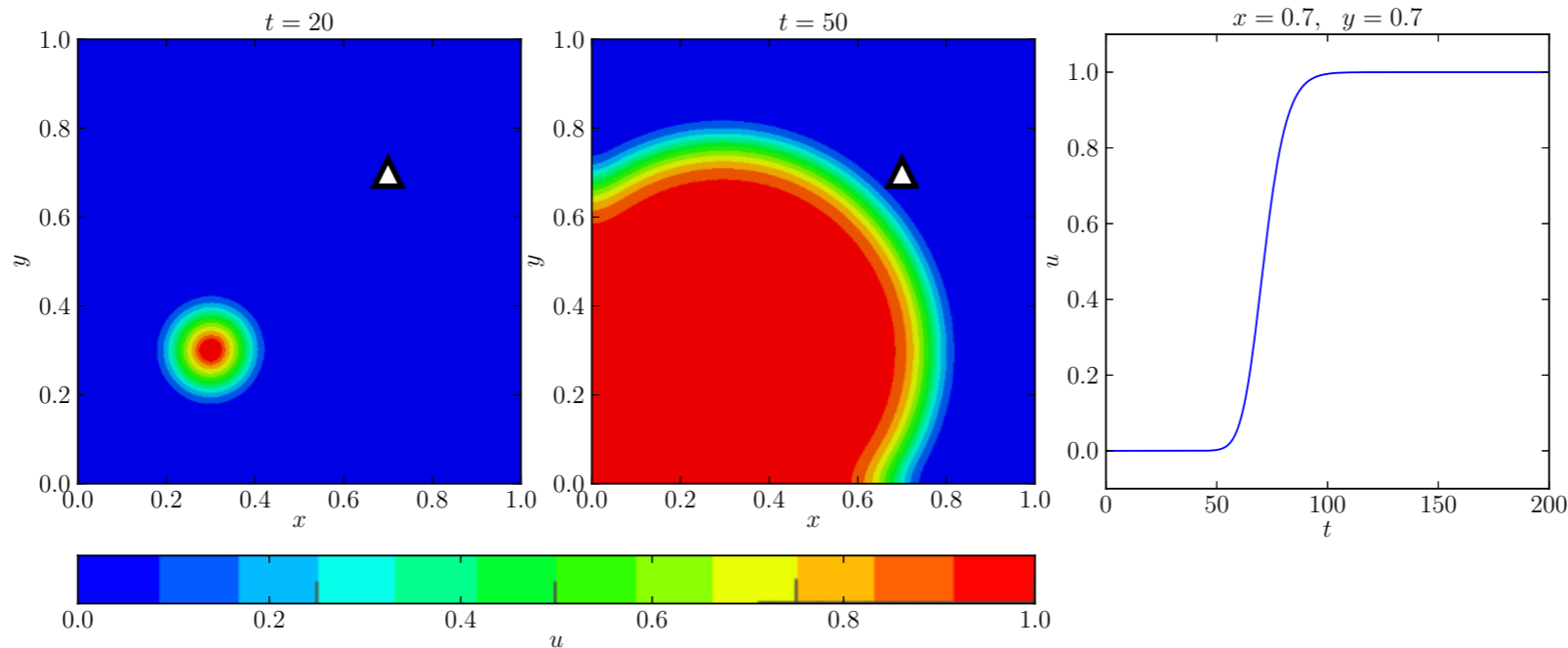
with

$$c_\rho(\mathbf{x}_j, m) = \mu_m^\rho(\mathbf{x}_j, m) - \hat{\mu}_m(\mathbf{x}_j, m)$$

- In practice  $n_{iter} \approx 3$

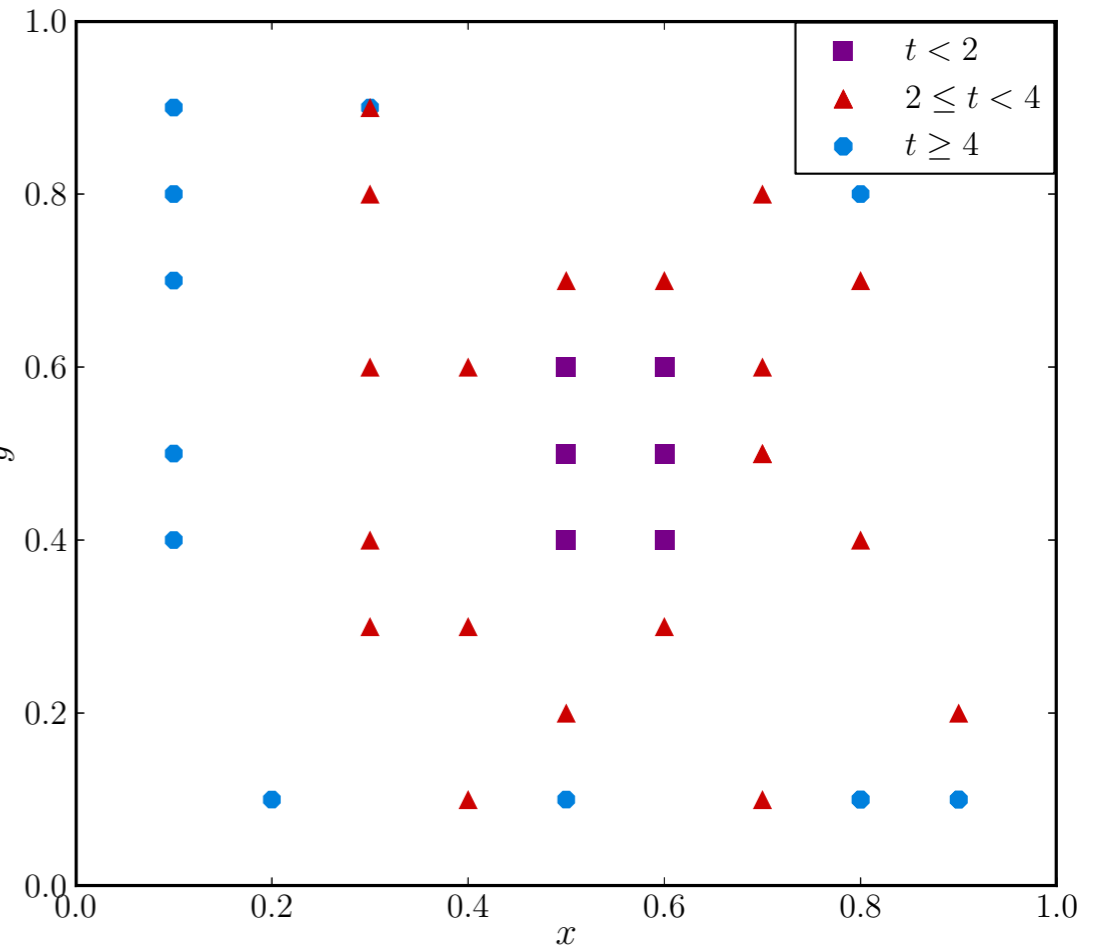
# Example 1: Fisher-Kolmogorov

- Nonlinear parabolic equation:  $\frac{\partial u}{\partial t} - \underbrace{\alpha \Delta u}_{\text{diffusion}} = \underbrace{Ru(1-u)}_{\text{reaction}} + \underbrace{f(\mathbf{x}, t)}_{\text{stimulation}}$

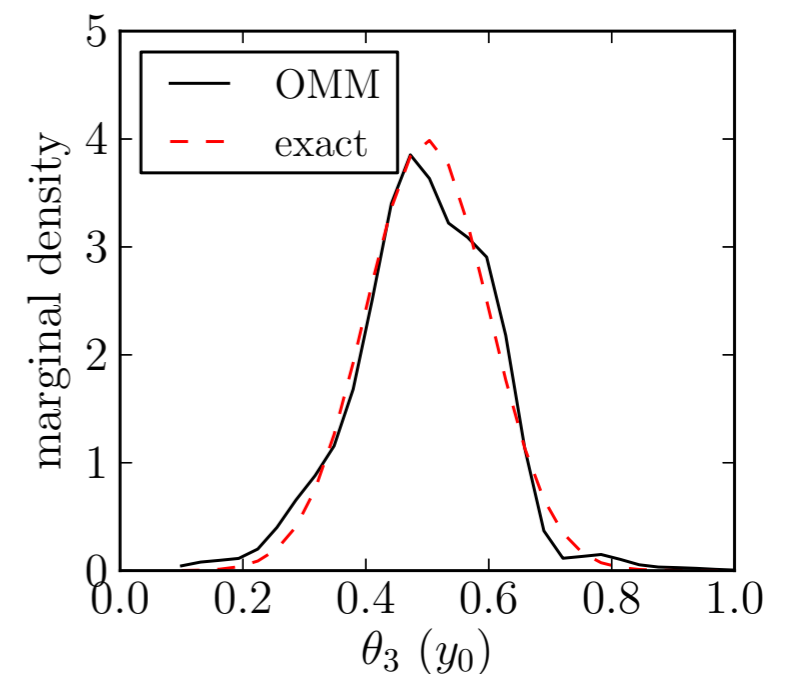
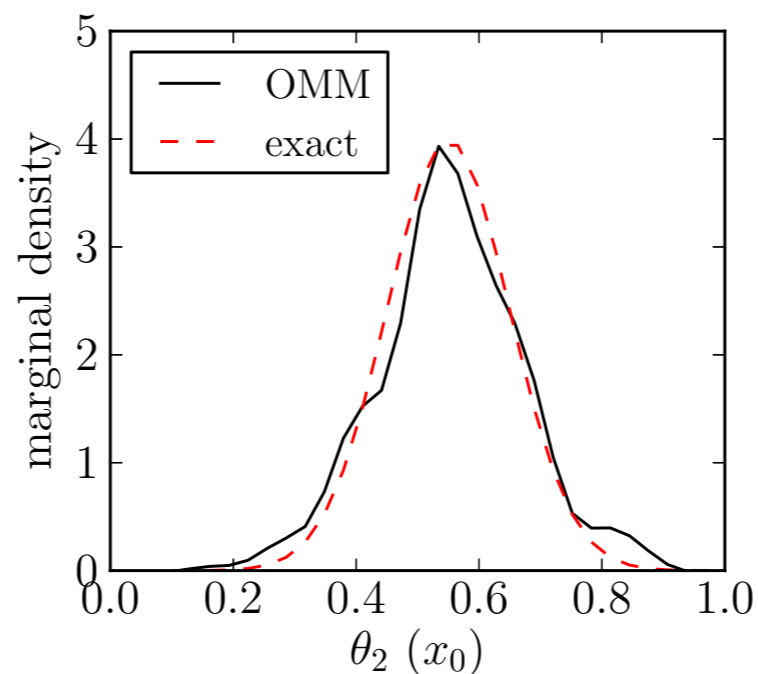
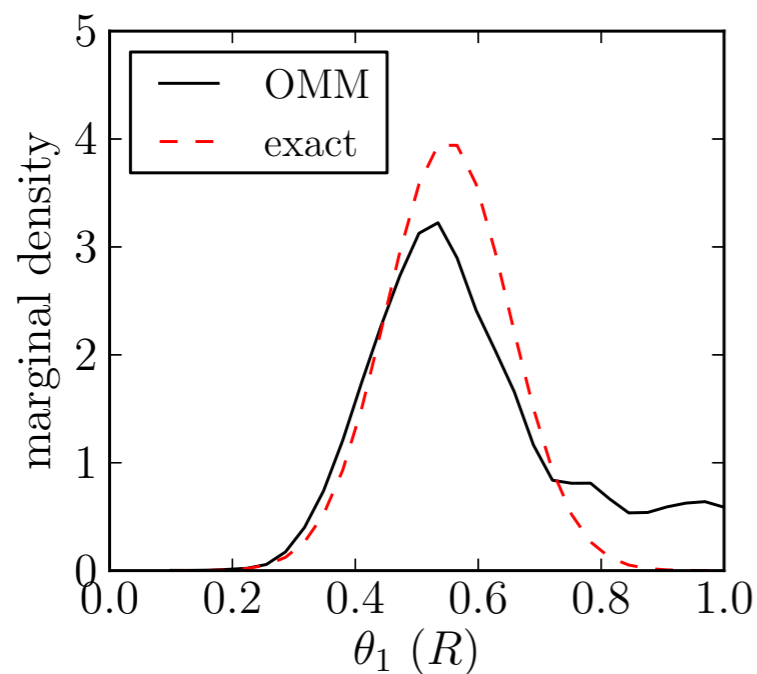


- 3 parameters responsible for variability:  
 $x_0, y_0$  (stimulation position) and  $R$  (reaction)
- Measurements:  $N_x = 81$  points in space  $\times$  200 time instants
- Synthetic data:  $10^3$  parameters sampled from a normal distribution  
 $\mu = [0.55, 0.55, 0.50]$ ,  $\Sigma = \sigma^2 \times \mathbf{I}_3$ , with  $\sigma = 0.1$
- Model evaluated for each sample + noise addition + different mesh

- $N_c = 2048$  Sobol points over  $\Theta = [0.1, 1.0]^3_y$
- $n_{mom} = 3$
- $N_k = 48$  selected space-time points
- $n_{iter} = 3$  iterations



Selected points



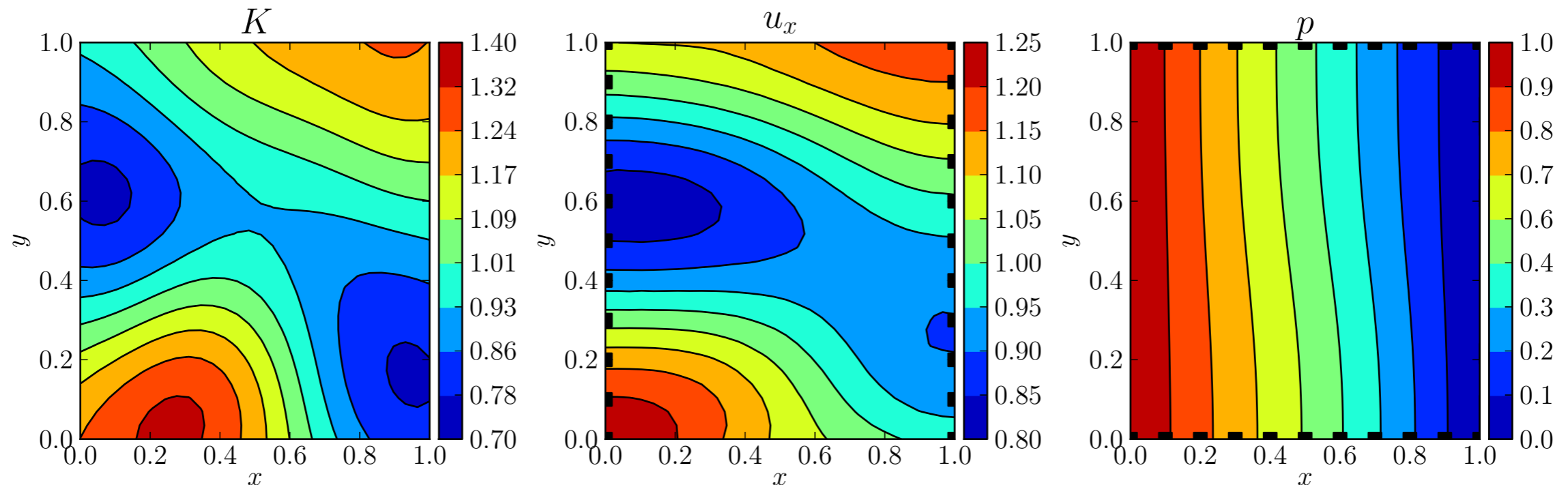
# Example 2: Darcy equation

- Darcy equation:

$$\begin{cases} \mathbf{u} + K \nabla p & = 0 \\ \operatorname{div} \mathbf{u} & = 0, \end{cases}$$

- Measurements:  $p$  and  $u_x$  on domain boundaries
- Variability: 5 coefficients  $\theta_k$  defining the permeability

$$K(x, y) = 1 + \sum_{k=1}^5 \theta_k \Psi_k(x, y)$$



- Synthetic data:

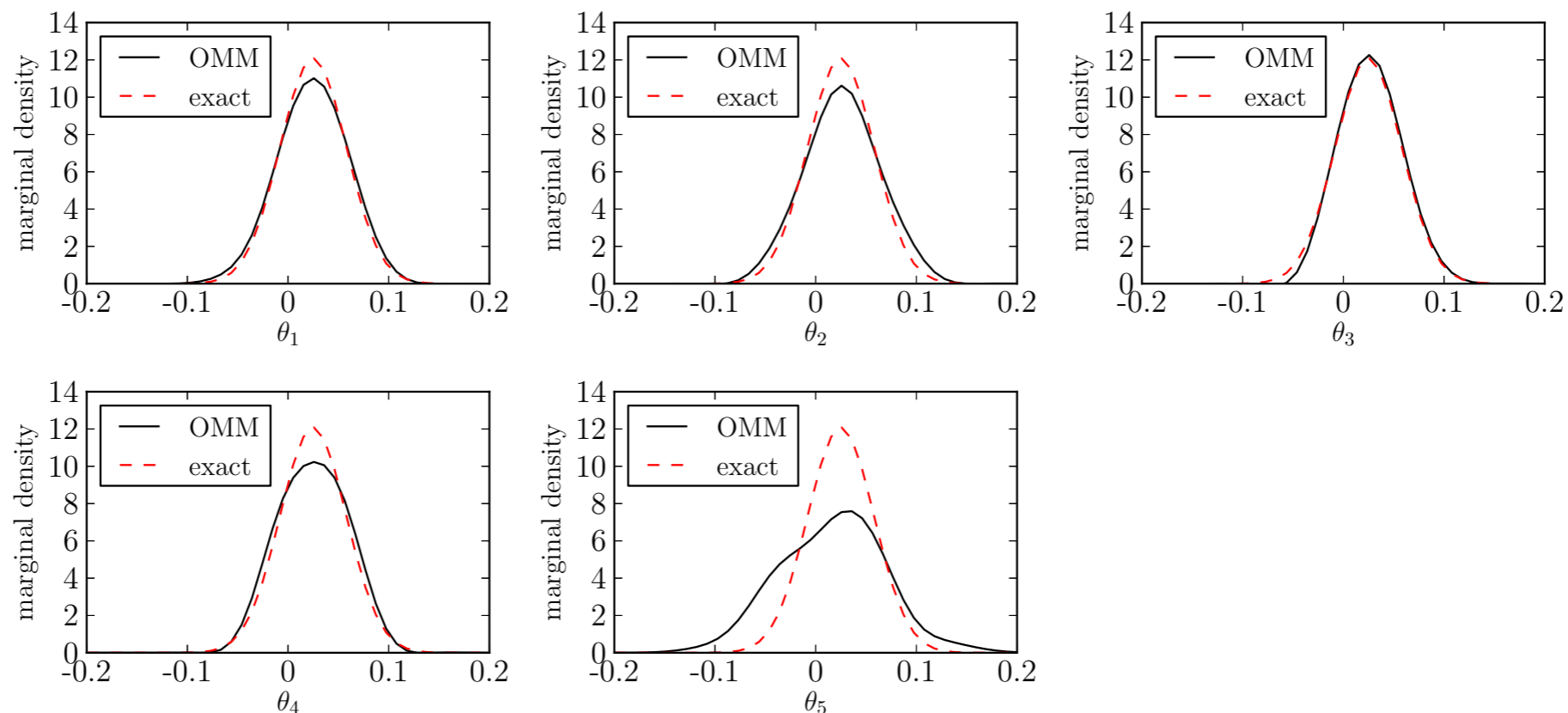
Evaluation of the model for  $N = 10^4$  samples of  $\theta = (\theta_1, \dots, \theta_5)$ .  
drawn from an uncorrelated multivariate normal distribution  
 $\mu = 2.5 \cdot 10^{-2} \times [1, 1, 1, 1, 1]$ ,  $\Sigma = \sigma^2 \times \mathbf{I}_5$ ,  $\sigma = 3.3 \cdot 10^{-2}$ .

- Moment matching algorithm:

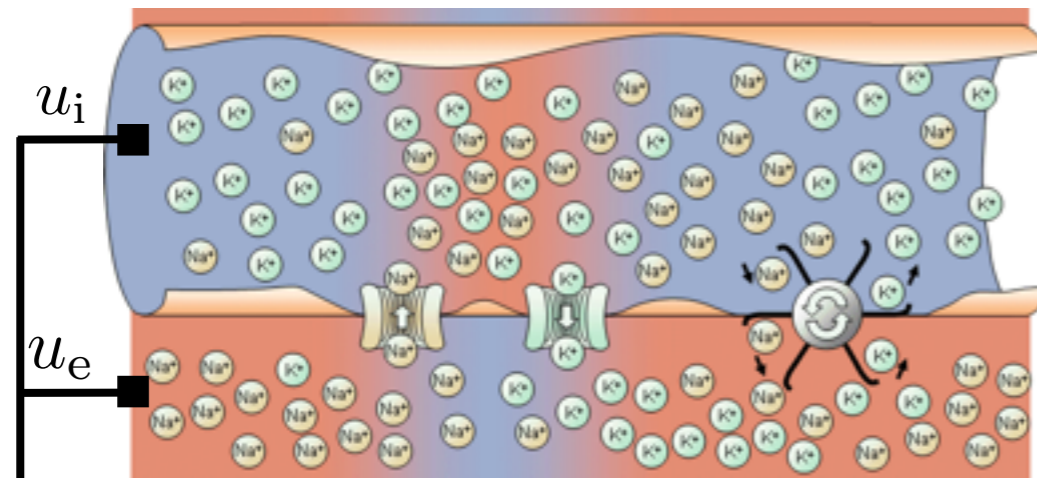
$N_c = 16384$  Sobol points over  $\Theta = [-0.2, 0.2]^5$

$n_{mom} = 3$

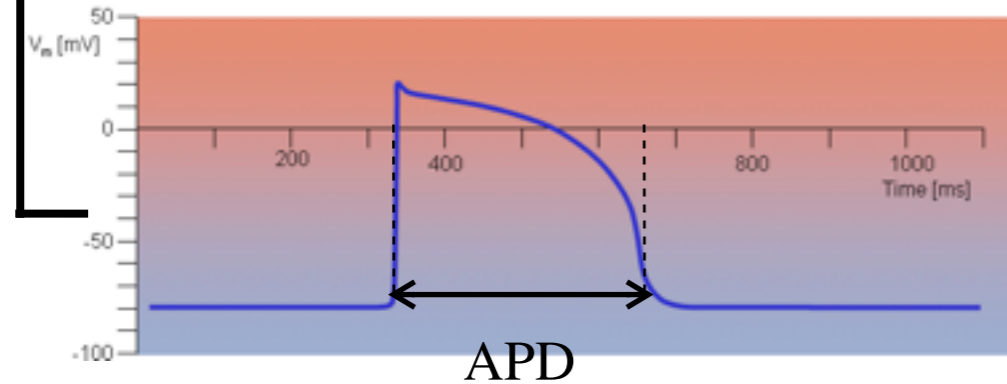
25 points selected by the Clustered Sensitivities algorithm (out of 400 sensors)



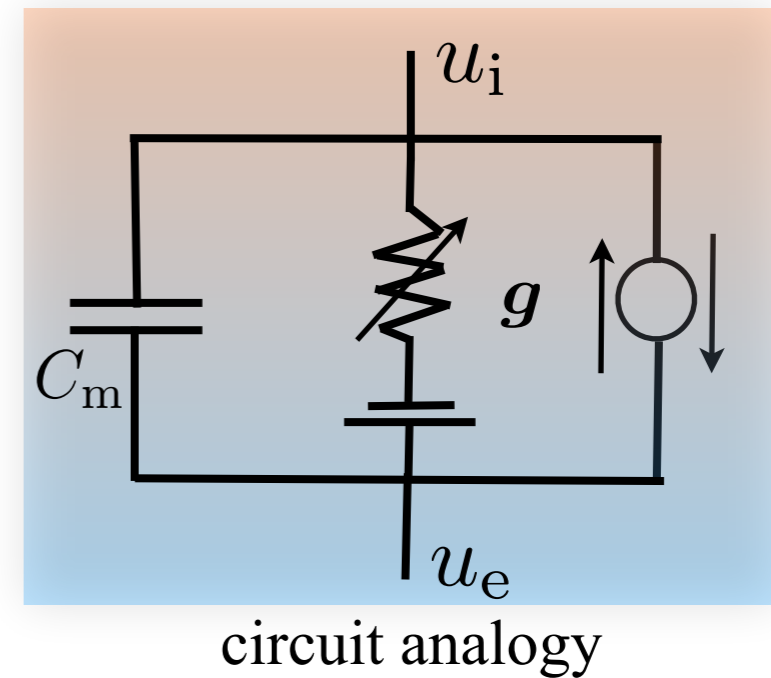
# Cardiac cell model



intracellular  
medium  
membrane  
extracellular  
medium



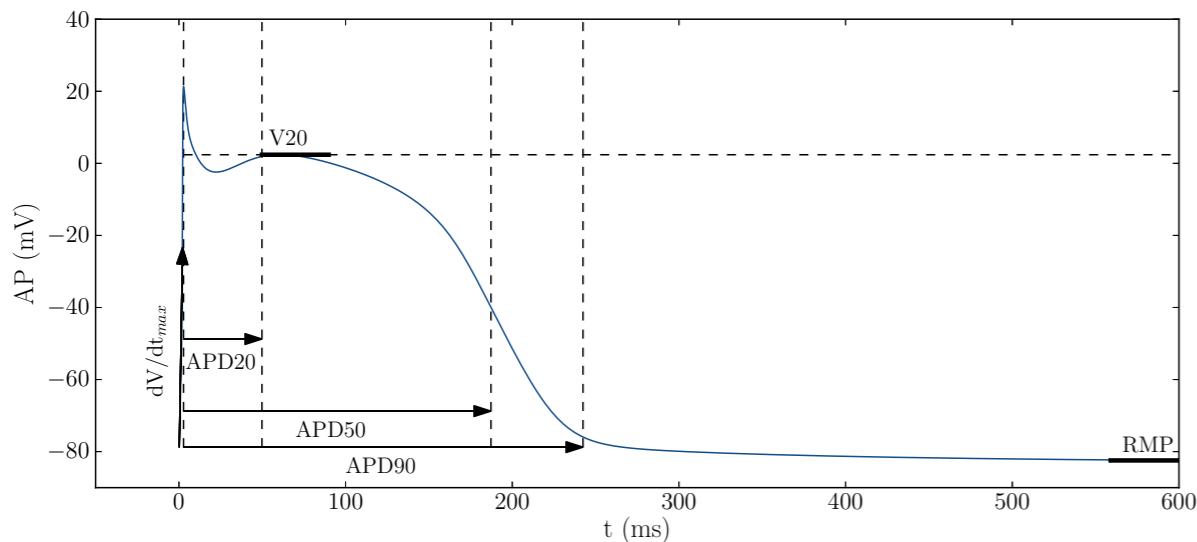
Extra-cellular potential:  $u_i$   
Extra-cellular potential:  $u_e$



circuit analogy

Action potential :  $V_m = u_i - u_e$

Biomarkers :

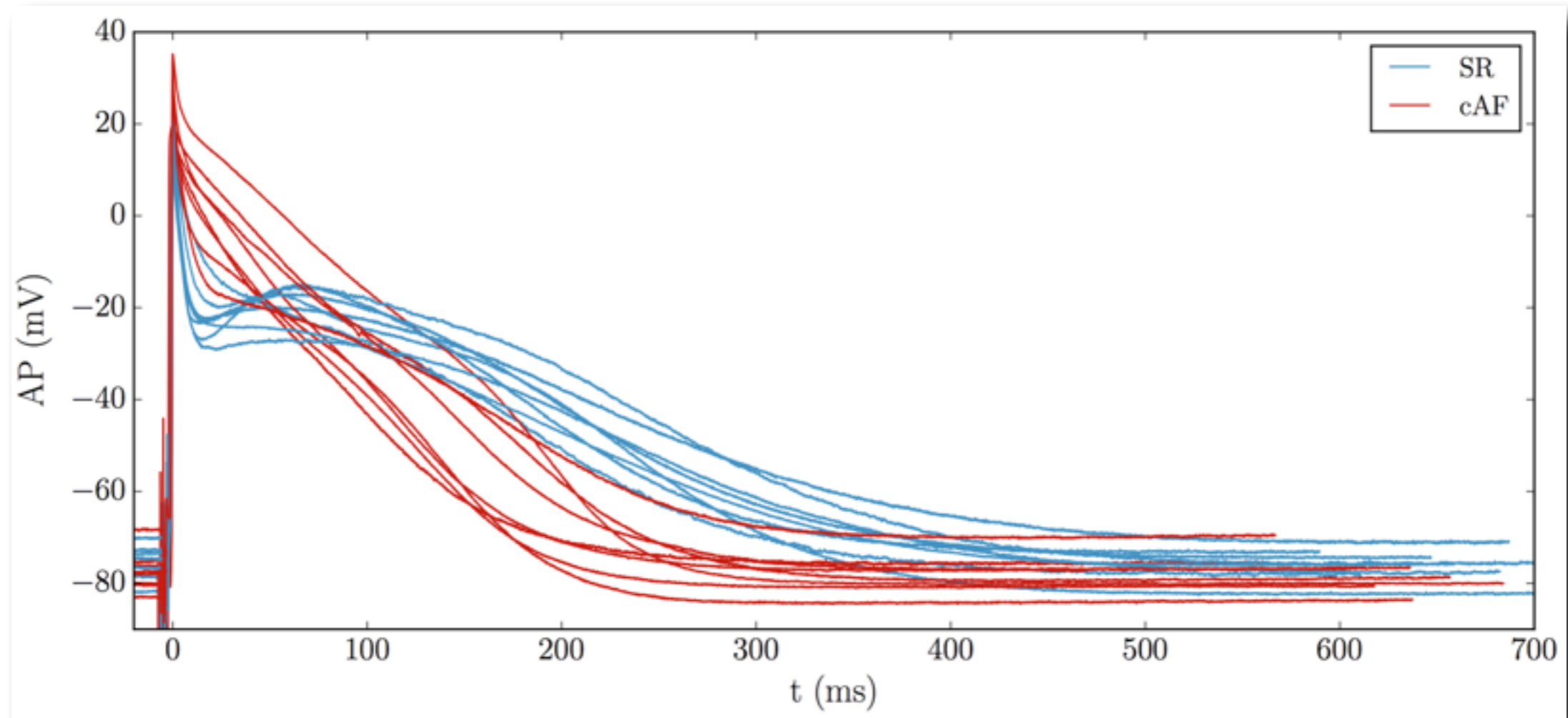


$$\begin{cases} C_m \frac{dV_m}{dt} + I_{\text{ion}}(V_m, \mathbf{g}) = 0 \\ \frac{d\mathbf{g}}{dt} + G(V_m, \mathbf{g}) = \mathbf{0} \end{cases}$$

(Hodgkin-Huxley 52, Cronin 81, Pullan et al. 05, Sunders et al. 06,...)



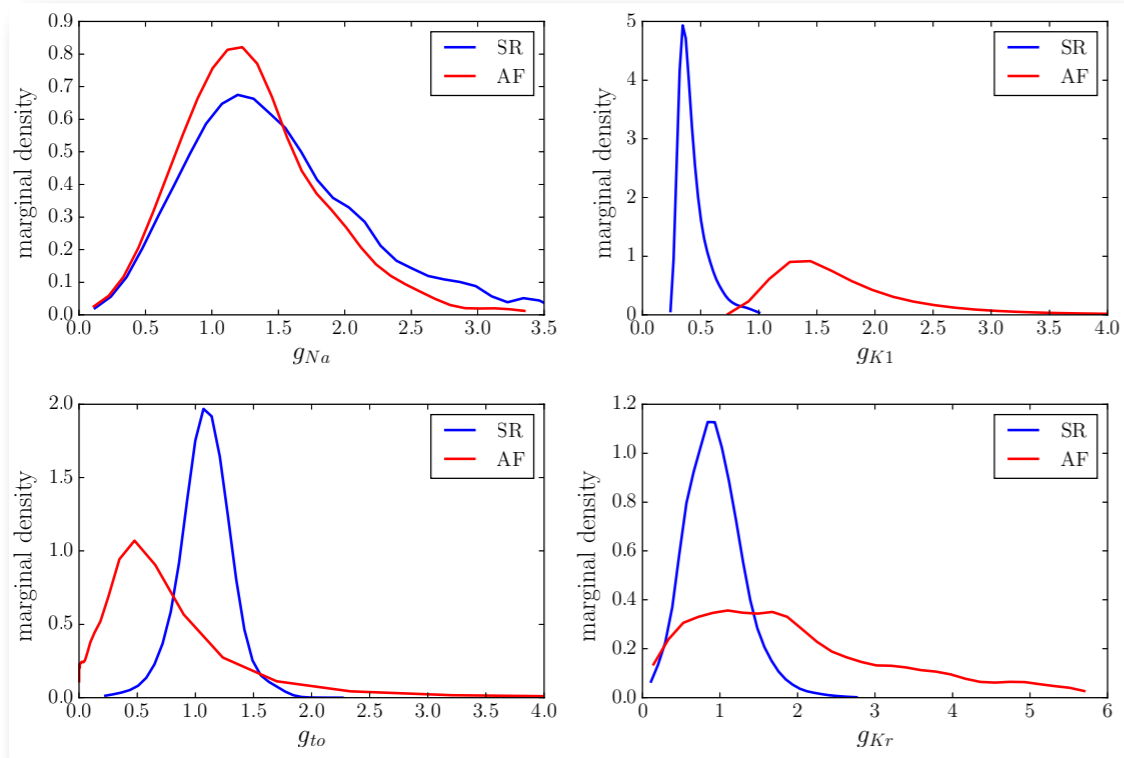
# Example 3: atrial fibrillation



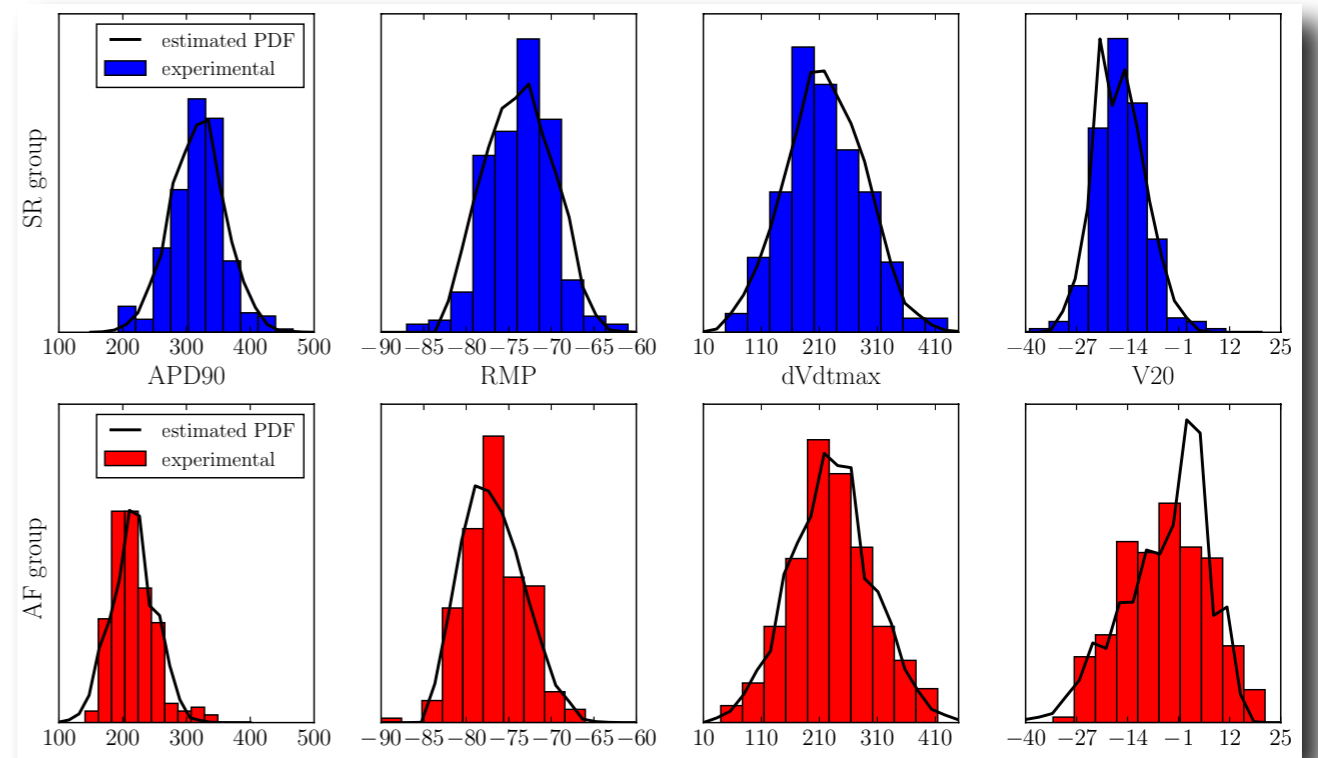
- Measurements from 2 populations: healthy (SR), atrial fibrillation (AF)
- Observable: set of AP features (4 biomarkers) for 469 subjects
- Strong inter-subject variability



*Sanchez et al.*, “Inter-Subject Variability in Human Atrial Action Potential in Sinus Rhythm versus Chronic Atrial Fibrillation”, [Plos One \(2014\)](#).



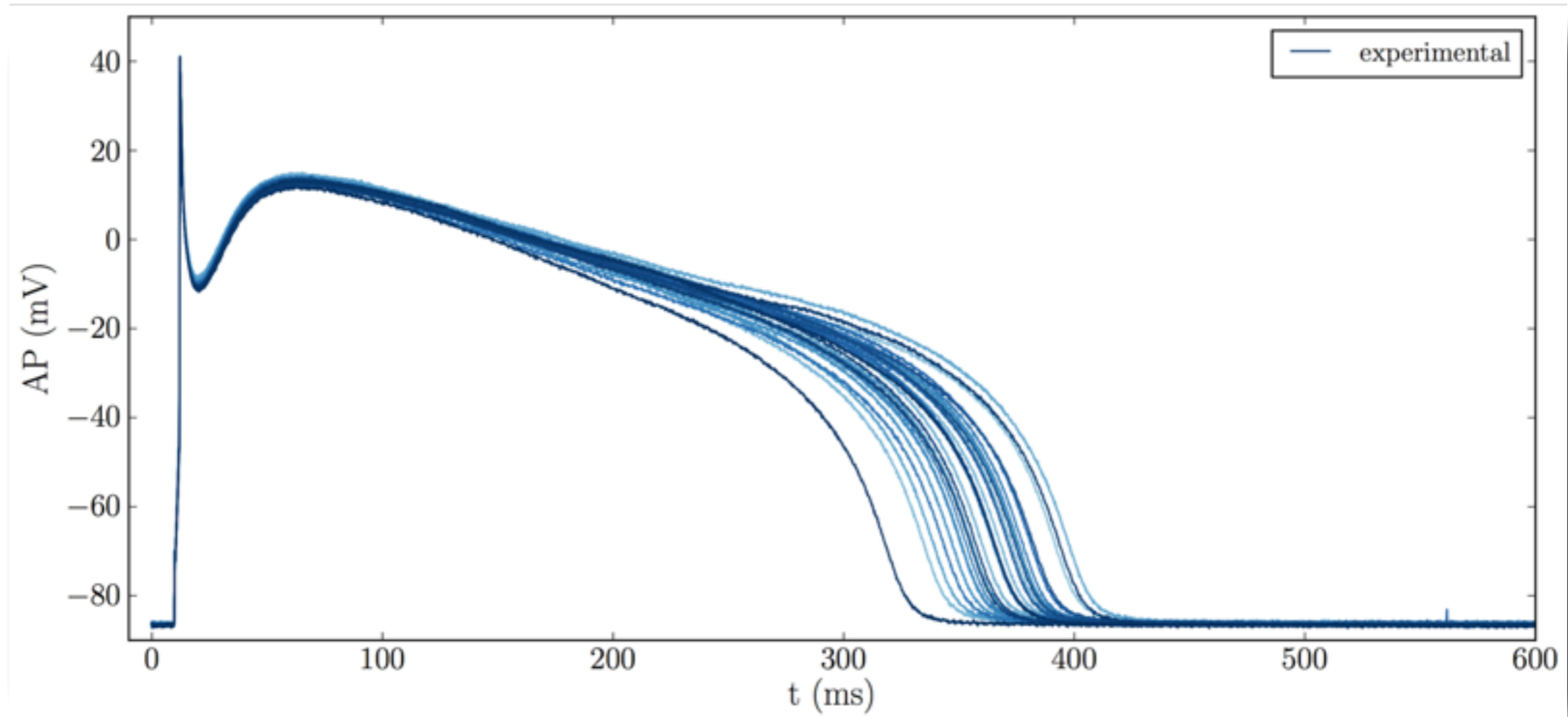
Distribution of 4 parameters  
(healthy and pathological)



Distribution of the biomarkers  
(estimated and experimental)

- Model: Courtemanche-Ramirez
- # samples:  $N_c = 16384$ ; # moments:  $n_{mom} = 2$ ; # clusters:  $N_k = 6$

# Example 4: Canine Action Potential

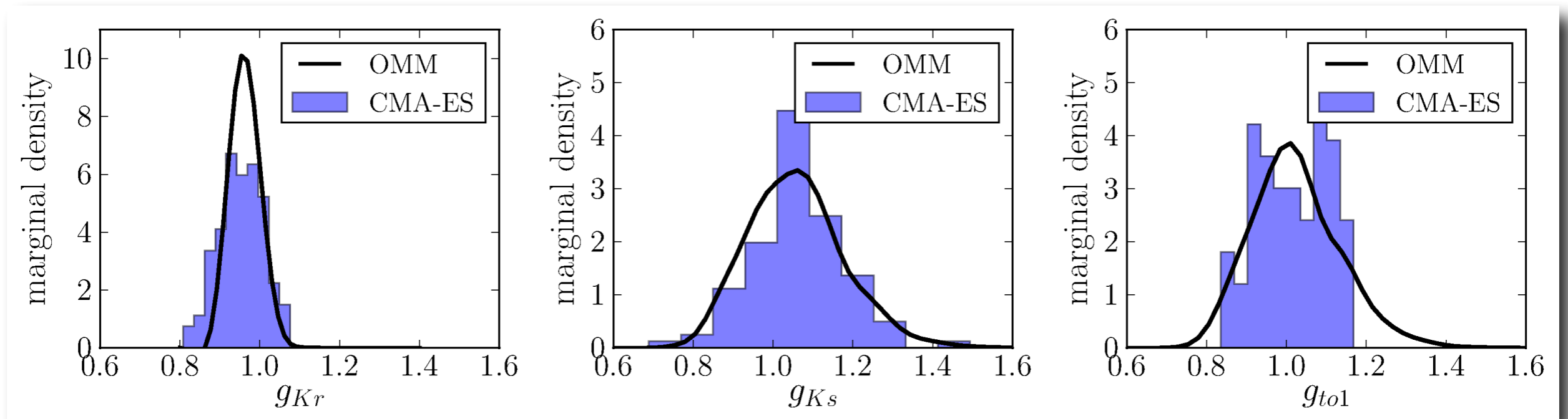


Samples of canine ventricular AP experimental recordings

- Measurements (100 APs) from canine heart cells
- Observable: set of AP features (biomarkers)
- Beat-to-beat variability



[Johnstone et al.](#), “Uncertainty and variability in models of the cardiac action potential: Can we build trustworthy models?”, *J. of Molecular and Cellular Cardiology* (2015).



Marginal distributions of 3 parameters estimated from experimental data.

- Model: Davies
- Hypothesis: only 3 parameters responsible for the variability
- Validation with individual parameter identification (evolutionary algo: CMA-ES)
- # samples:  $N_c = 8192$ ; # moments:  $n_{mom} = 2$ ; # clusters:  $N_k = 3$

# Conclusions & Perspectives

## Summary

- Approximate parameters distribution from observed variability in a population
- Non-parametric and black-box approach
- Tested with synthetic & experimental data

## Perspectives

- How to determine which parameters are responsible for variability?
- What to do with the remaining parameters?
- How to choose relevant biomarkers? [**Elliott Tixier's talk**]
- Use the obtained distribution as a *prior* for more sophisticated inverse problem algorithms



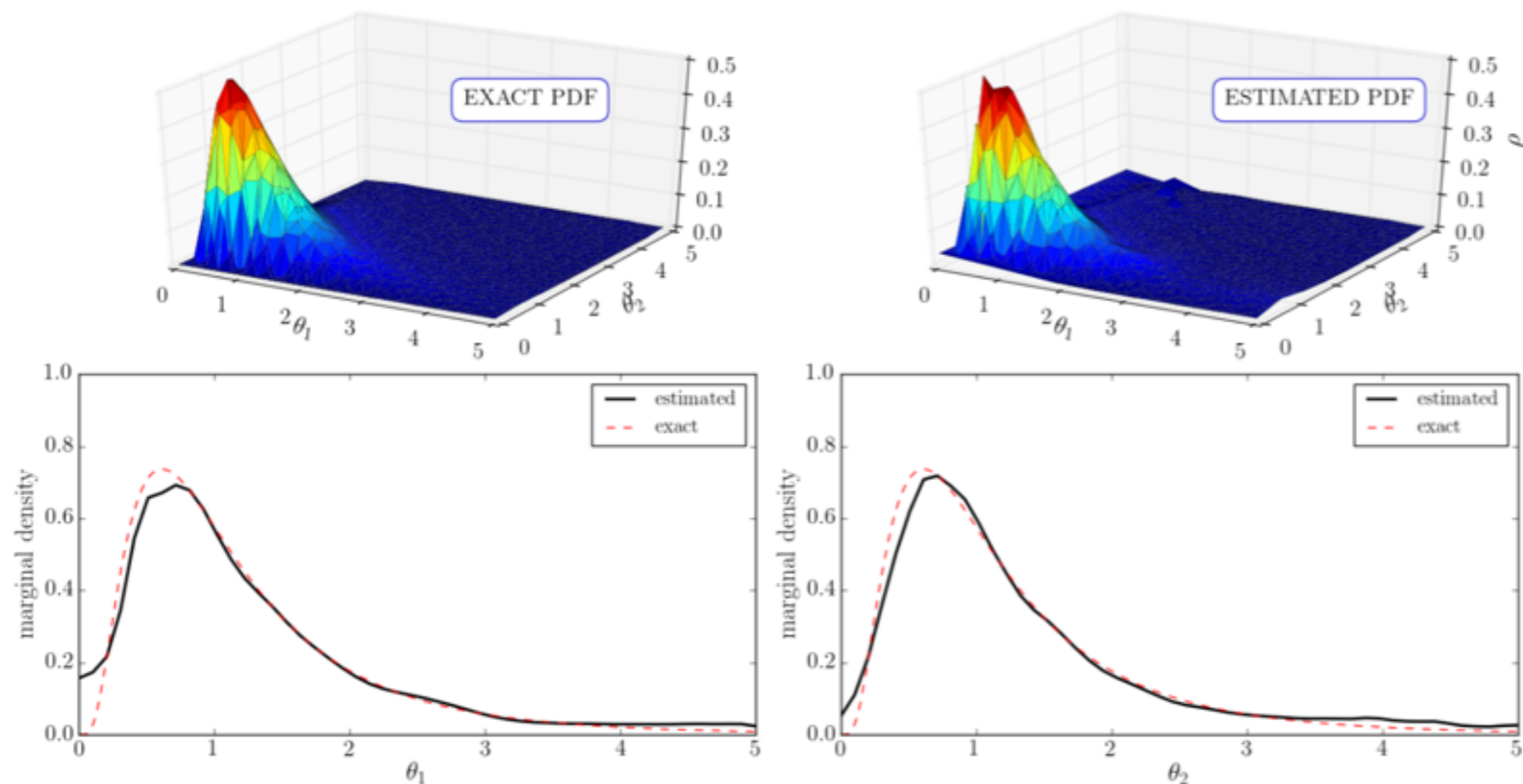
J-F. Gerbeau, D. Lombardi, E. Tixier, “A moment-matching method to study the variability of phenomena described by partial differential equations”, available on HAL: <https://hal.archives-ouvertes.fr/hal-01391254/>



E. Tixier, D. Lombardi, B. Rodriguez, J-F. Gerbeau, “Modeling Variability in Cardiac Electrophysiology: A Moment Matching Approach”, [Journal of the Royal Society Interface](#) (2017).

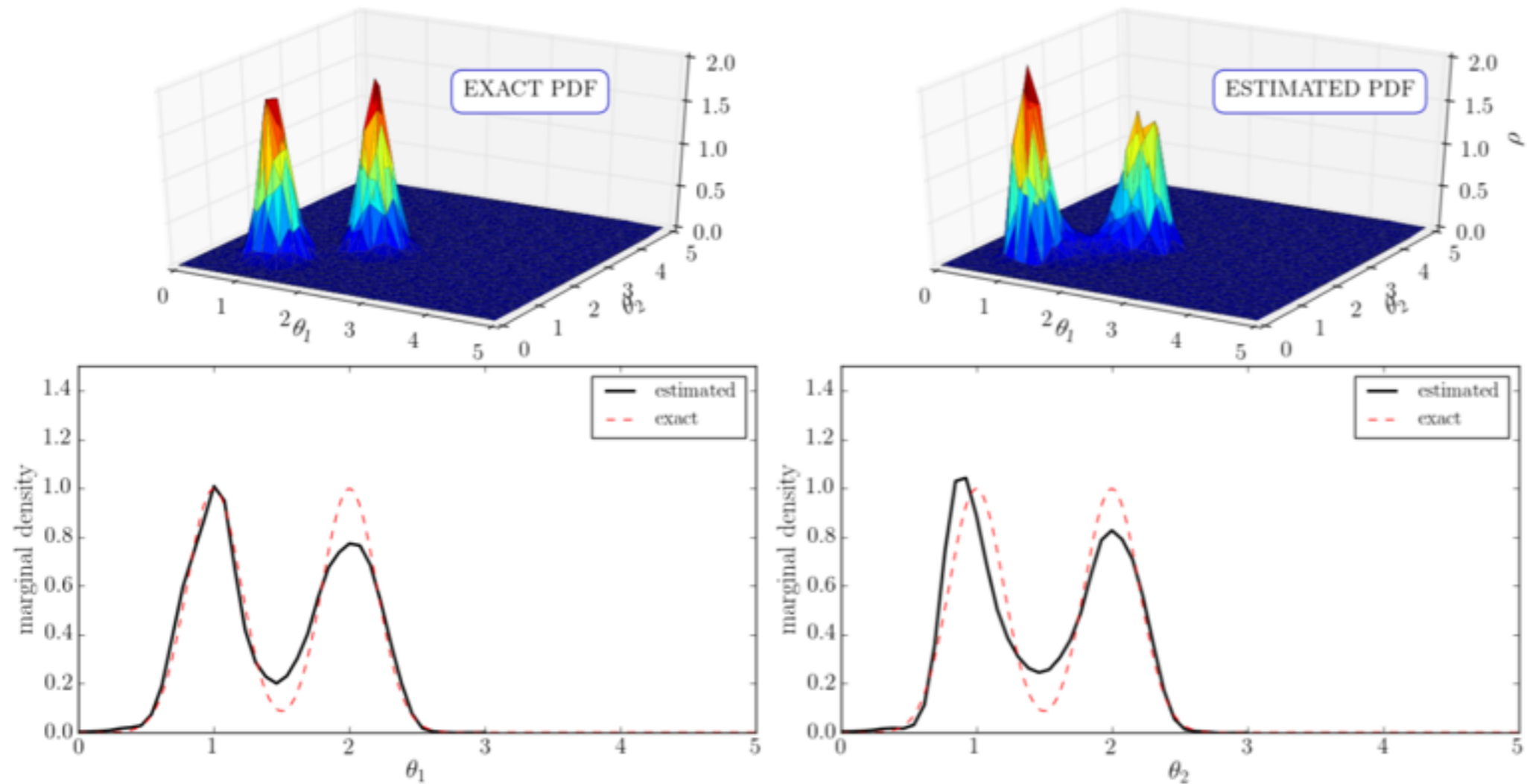
- You can test it: [https://github.com/eltix/omm\\_jrsi.git](https://github.com/eltix/omm_jrsi.git)

- Bi-variate **log-normal** distribution
- Strongly skewed
- Numerical settings:  $N_C = 2048$ ,  $n_{mom} = 4$  and  $N_x = 10$



Observable moment matching applied to synthetic data. Log-normal distribution

- Gaussian mixture **bimodal** distribution
- $\theta_1$  and  $\theta_2$  are strongly correlated
- Numerical settings:  $N_C = 2048$ ,  $n_{mom} = 4$ ,  $N_x = 16$



Observable moment matching applied to synthetic data. Bimodal distribution